OpenGLSL-based Raycasting Comparison of Execution Durations of Multi-pass vs. Single-pass Technique

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Abstract: Real time volume rendering of medical datasets using raycasting on graphics processing units (GPUs) is a common technique. Since more than 10 years there are two established approaches for realizing GPU ray casting: multi-pass (Kruger and Westermann, 2003) and single-pass (Röttger, et al., 2003). But the required parameters to choose the optimal raycasting technique for a given application are still unknown. To solve this issue both raycasting techniques were implemented for different raycasting types using OpenGLSL vertex and fragment shaders. The different techniques and types were compared regarding execution times. The results of this comparison show that there is no technique faster in general. The higher the computational load the more indicates the use of the multi-pass technique.

1 INTRODUCTION

In the last few years GPUs have become the most important means for direct volume rendering (DVR). Raycasting is the state of the art technique for realizing DVR on GPUs (Marques, et al., 2009), (Mensmann, et al., 2010). There are two basic approaches for realizing GPU raycasting: multi-pass and single-pass. These approaches differ in how they calculate the ray marching direction vectors.

The multi-pass approach, as implemented by (Kruger & Westermann, 2003) works as follows when using OpenGLSL vertex and fragment shaders:

A volume dataset is stored in the graphics memory as a 3-D texture. 3-D textures are indexed with texture coordinates

 $(x_coord, y_coord, z_coord) \in [0.0, 1.0].$ (1)

The next steps are:

Pass 1: The front facing faces of the volume bounding box are rendered to a texture with 3-D texture coordinates (1) as RGB-encoded color values. These coordinates are the ray start positions for the raycasting.

Pass 2: The back facing faces of the volume bounding box are rendered to another texture with 3-D texture coordinates (1) as encoded color values. These coordinates are the ray exit positions for the raycasting. Based on the coordinate information of passes 1 and 2, the ray directions can be calculated. The directions are rendered as color to another 3-D texture for use in the last pass.

Pass 3: The raycasting is performed by a fragment shader casting each ray along the calculated direction through the volume using a given step size.

The single-pass approach (Röttger, et al., 2003) uses only a fragment shader to calculate the ray entry and exit points and performs the raycasting (figure 1). The ray directions are calculated by subtracting the vertex position from the camera position. The ray entry positions are the positions of the front vertices. From here the raycasting performs like in pass 3 of multi-pass raycasting until the ray exits the volume.



Figure 1: Single-pass raycasting (Movania, 2013).

The advantage of single-pass raycasting is its simplicity. Due to the reduction of textures and

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saving of many OpenGL calls regarding the volume bounding box creation, it should be faster than multi-pass raycasting. The disadvantage is the full computational load on the fragment shader (Venkataraman, 2009) which could slow down the raycasting.

Different optimization techniques can be implemented to lower execution times (ETs). One of the most common techniques is the "Early Ray Termination" (ERT) (Matsui, et al., 2005). It was implemented because of its high potential of lowering the ET while being easy to realize in OpenGLSL.

Currently the required parameters to choose the optimal raycasting technique for a given application are unknown. The comparison reported here shall be a first contribution to clarify this issue.

2 MATERIALS AND METHODS

Both raycasting techniques were implemented using C# and OpenGLSL 4.3 (with OpenGL4Net (Vanecek, 2014)). The engaged hardware consists of a notebook (Windows 7 SP1, Intel Core i5-4200M CPU, 2.5 GHz, 16 GB RAM) with an NVIDIA Quadro K3100M (driver version 312.32) graphics card. The raycasting is performed using an ultrasound image volume with 512×378×222 grayscale values (8bit, unsigned integer), a voxel spacing of 0.42 mm×0.39 mm×0.63 mm and a viewport size of 1440×900.

For the comparison three different raycasting types were implemented with and without ERT.

- "Minimum Intensity Projection" (MINIP) (Radiopaedia.org, 2014) - a simple rendering technique to visualize e.g. liver vessels in ultrasound volumes (figure 2) – as a technique with low computing time.
- 2. Alpha Blending (Porter & Duff, 1984) as a technique with medium computing time.
- 3. Gradient Calculation using the left and right neighbor of each pixel along the ray as a technique with high computing time due to many texture fetches.

To measure the ET of the raycasting techniques the following steps were realized:

- 1. Implement both raycasting techniques as described above.
- Implement in-application profiling using OpenGL "elapsed time queries" (Shreiner, et al., 2013)
 - a. Single-pass: At the end of each "paint"-call

- b. Multi-pass: At the end of the volume bounding box building and at the end of each "paint"-call
- 3. Load the ultrasound dataset.
- 4. Choose the raycasting type.
- 5. Activate or deactivate ERT.
- 6. Set the step size to a defined value from 0.001 to 0.05 mm (table 1).
- Perform an arc shot with an angular step size of 1 (= sum of 360 steps) and call "paint" after each angular step.
- 8. Repeat step 5 ten times to have a sum of 3600 (single-pass) respectively 7200 (multi-pass) profiling values per step size.
- 9. Average the ETs and add them to table 1.
- 10. Repeat step 4 to 9 for every raycasting type.



Figure 2: Ultrasound volume visualization (MINIP) of liver vessels.

3 RESULTS

The results of the ET measurements for the three raycasting types can be seen in tables 1 to 3. To show the change of ET ratio, the quotients of multipass ETs divided by single-pass ETs were calculated.

Table 1: MINIP ET (times in milliseconds).

MINIP							
step size	single-pass		multi-pass		quotient		
[mm]	raycast	ERT	raycast	ERT	raycast	ERT	
0.001	226.3	180.4	126.0	101.4	0.6	0.6	
0.002	118.7	99.1	78.6	67.8	0.7	0.7	
0.005	49.3	43.8	47.6	43.3	1.0	1.0	
0.01	26.6	23.5	36.8	33.7	1.4	1.4	
0.02	15.5	14.1	30.5	28.4	2.0	2.0	
0.05	8.6	8.6	27.9	26.0	3.2	3.0	

Additionally the ETs and quotients of the MINIP results are shown exemplary in figure 3 (without ERT) and in figure 4 (with ERT).

As explained in the introduction the multi-pass raycasting consists of building the geometry first before executing the raycasting itself. Due to the fact that the geometry building remains almost constant at about 0.5 to 0.6 milliseconds it is not included separately in the tables and figures. (The multi-pass execution times are the sum of all passes.)



Figure 3: ETs over step sizes (MINIP, without ERT) and the quotient of multi-pass divided by single-pass times.

Table 2: Alpha Blending ET (times in milliseconds).

Alpha Blending							
step size	single-pass		multi-pass		quotient		
[mm]	raycast	ERT	raycast	ERT	raycast	ERT	
0.001	275.2	147.3	117.2	76.3	0.4	0.5	
0.002	146.2	81.9	73.6	52.2	0.5	0.6	
0.005	63.0	38.0	44.7	37.1	0.7	1.0	
0.01	33.8	21.0	35.0	31.8	1.0	1.5	
0.02	18.3	12.5	28.7	28.5	1.6	2.3	
0.05	9.8	8.4	26.8	26.4	2.7	3.1	

Table 3: Gradient Calculation ET (times in milliseconds).

Gradient Calculation							
step size	single-pass		multi-pass		quotient		
[mm]	raycast	ERT	raycast	ERT	raycast	ERT	
0.001	369.5	52.2	408.5	159.1	1.1	3.0	
0.002	194.5	31.1	240.0	101.6	1.2	3.3	
0.005	83.5	17.3	123.5	66.4	1.5	3.8	
0.01	46.6	13.6	77.2	52.7	1.7	3.9	
0.02	27.0	11.0	53.3	44.0	2.0	4.0	
0.05	13.3	9.5	37.0	36.1	2.8	3.8	



Figure 4: ETs over step sizes (MINIP, with ERT) and the quotient of multi-pass divided by single-pass times.

4 DISCUSSION

The results show that the ERT can lower the ET up to about 14% in the best case (Gradient Calculation, single-pass, step size 0.001). At worst the ERT had no influence on the ET (MINIP, single-pass, step size 0.05). Hence the implementation of an ERT is always advisable.

Furthermore the results show that the single-pass implementation produces lower ETs than the multipass one at step sizes larger than about 0.005 mm for the MINIP (with and without ERT) and 0.01 mm for the Alpha Blending (with and without ERT).

For the Gradient Calculation the results show that the single-pass raycasting produces lower ETs for the whole measurement. But the quotient reveals that the multi-pass raycasting would produce lower ETs for even smaller step sizes.

Smaller step sizes lead to higher computational load for the fragment shader. As remarked in the introduction the full computational load of the fragment shader is the disadvantage of the singlepass technique. When this load reaches a certain value the performance lead changes from single-pass technique to multi-pass technique.

Therefore, the reported comparison shows that there is no general performance advantage for one of the raycasting techniques. The ET of the respective technique depends on the computational load of the fragment shader and on the chosen raycasting type.

Further work is addressed to the determination of the exact parameters that define which raycasting technique should be preferred for which task. Additionally the influence of more optimization

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techniques (e.g. empty space skipping, culling techniques) and the used graphics card will be investigated.

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REFERENCES

- Kruger, J. and Westermann, R., 2003. Acceleration Techniques for GPU-based Volume Rendering. *Proceedings of the 14th IEEE Visualization 2003* (VIS'03), p. 38.
- Marques, R., Santos, L. P., Leskovsky, P. and Paloc, C., 2009. GPU ray casting. Proceedings of the 17th Encontro Portugeês de Computação Gráfica (EPCG 09), p. 83–91.
- 09), p. 83–91.
 Matsui, M., Ino, F. and Hagihara, K., 2005. Parallel Volume Rendering with Early Ray Termination for Visualizing Large-Scale Datasets. *Parallel and Distributed Processing and Applications*, pp. 245-256.
- Mensmann, J., Ropinski, T. and Hinrichs, K., 2010. An Advanced Volume Raycasting Technique using GPU Stream Processing. *GRAPP: International Conference* on Computer Graphics Theory and Applications, pp. 190-198.
- Movania, M. M., 2013. OpenGL Development Cookbook. Birmingham, UK: Packt Publishing.
- Porter, T. and Duff, T., 1984. Compositing Digital Images. SIGGRAPH Comput. Graph., July, pp. 253-259.
- Radiopaedia.org, 2014. Radiopaedia. [Online] Available at: http://radiopaedia.org/articles/minimum-intensityprojection-minip [Accessed 11/16/2014].
- Röttger, S. et al., 2003. Smart Hardware-Accelerated Volume Rendering. *Proceedings of EG/IEEE TCVG Symposium on Visualization*, pp. 231-238.
- Shreiner, D., Sellers, G., Kessenich, J. and Licea-Kane, B., 2013. In-Application Profiling. In: OpenGL Programming Guide, Eighth Edition. Upper Saddle River, NJ et al.: Addison-Wesley, pp. 881-883.
- Vanecek, 2014. OpenGL4Net. [Online] Available at: http://sourceforge.net/projects/ogl4net/ [Accessed 11/16/2014].
- Venkataraman, S., 2009. 4D Volume Rendering. Silicon Valley, s.n.