Efficient and Accurate Hyperspectral Image Demosaicing with Neural Network Architectures

Eric L. Wisotzky^{1,2}[®], Lara Wallburg¹, Anna Hilsmann¹[®], Peter Eisert^{1,2}[®],

Thomas Wittenberg^{3,4} and Stephan Göb^{3,4} ^[D]

¹Computer Vision & Graphics, Fraunhofer HHI, Einsteinufer 37, 10587 Berlin, Germany

²Department of Informatics, Humboldt University, Berlin, Germany

³Fraunhofer IIS, Erlangen, Germany

⁴Chair of Visual Computing, Friedrich-Alexander-Universität Erlangen-Nürnberg, Erlangen, Germany

Keywords: Sensor Array and Multichannel Signal Processing, Deep Learning, Biomedical Imaging Techniques, Image Analysis, Image Upsamling.

Abstract: Neural network architectures for image demosaicing have been become more and more complex. This results in long training periods of such deep networks and the size of the networks is huge. These two factors prevent practical implementation and usage of the networks in real-time platforms, which generally only have limited resources. This study investigates the effectiveness of neural network architectures in hyperspectral image demosaicing. We introduce a range of network models and modifications, and compare them with classical interpolation methods and existing reference network approaches. The aim is to identify robust and efficient performing network architectures. Our evaluation is conducted on two datasets, "SimpleData" and "SimReal-Data," representing different degrees of realism in multispectral filter array (MSFA) data. The results indicate that our networks outperform or match reference models in both datasets demonstrating exceptional performance. Notably, our approach focuses on achieving correct spectral reconstruction rather than just visual appeal, and this emphasis is supported by quantitative and qualitative assessments. Furthermore, our findings suggest that efficient demosaicing solutions, which require fewer parameters, are essential for practical applications. This research contributes valuable insights into hyperspectral imaging and its potential applications in various fields, including medical imaging.

1 INTRODUCTION

The use of multispectral images (MSIs) or hyperspectral images (HSIs), which encompass a wide range of different spectral channels across various wavelengths both within and beyond the visible spectrum, has gained increasing prominence in recent years. These types of images find broad applications in various fields such as healthcare (Calin et al., 2014; Lu and Fei, 2014; Zhang et al., 2017), industrial applications (Shafri et al., 2012), and agriculture (Jung et al., 2006; Moghadam et al., 2017). However, conventional acquisition methods and devices are associated with significant drawbacks, including high costs

and lengthy acquisition times (Wisotzky et al., 2018; Mühle et al., 2021).

In recent times, alternative approaches have been developed to address these challenges. One promising technique is based on the use of spectral masking at the pixel level, utilizing only a single sensor plane. This concept is known as Multi-Spectral Filter Arrays (MSFAs). Unlike RGB images, which are composed of three color values (red, green and blue), MSFAs map the spectrum in more than three spectral bands, e.g., nine, 16 or 25 bands (Hershey and Zhang, 2008). A data cube is formed from the determined data. Its edges represent the image dimensions in x- and y-direction and the determined wavelengths in λ -direction. In contrast to MSIs, HSIs use several hundred spectral bands to capture the spectrum of a source.

When image data is acquired by a multispectral camera using the principle of MSFA, not all image

Wisotzky, E., Wallburg, L., Hilsmann, A., Eisert, P., Wittenberg, T. and Göb, S.

Efficient and Accurate Hyperspectral Image Demosaicing with Neural Network Architectures.

DOI: 10.5220/0012392300003660

Paper published under CC license (CC BY-NC-ND 4.0)

^a https://orcid.org/0000-0001-5731-7058

^b https://orcid.org/0000-0002-2086-0951

^c https://orcid.org/0000-0001-8378-4805

^d https://orcid.org/0000-0002-1206-7478

In Proceedings of the 19th International Joint Conference on Computer Vision, Imaging and Computer Graphics Theory and Applications (VISIGRAPP 2024) - Volume 3: VISAPP, pages 541-550

ISBN: 978-989-758-679-8; ISSN: 2184-4321

information of a data cube can be acquired. An increase in spectral resolution is accompanied by a loss of spatial resolution. This missing information needs a successive interpolation using image processing or image analysis techniques. Common image processing techniques for spectral reconstruction include bilinear and nonlinear filters, referred to as debayering or demosaicing.

While MSFAs offer the advantage of real-time implementation and general applicability, accurate interpolation of missing spectral or spatial information is challenging. This, however, is crucial for precise spatial localization of entities such as cancer cells in healthcare, damage in plants in agriculture, or objects in industrial applications. To enhance existing methods, neural networks have recently been proposed as promising approaches.



Figure 1: Description of the processing pipeline and demosaicing of multispectral cameras.

The contribution of this work is as follows. We present a pipeline to achieve real-world MSFA data from different hyperspectral datasets. Further, we propose different new and extended demosaicing networks and compare these using classical public available datasets and a dataset processed with our introduced pipeline.

The analysis is performed from the perspective that the networks should provide good reconstruction quality and be able to compute it quickly, i.e., contain as few parameters as possible for potential nearsensor processing.

The remainder of this paper is as follows. The next chapter gives an overview on related publications relevant for this work. Chapter 3 describes the proposed network architectures, before chapter 4 explains data processing and presents training and evaluation parameters. Chapter 5 describes experiments and results, followed by a thorough discussion and conclusion.

2 RELATED WORK

The most commonly used algorithms for demosaicing in imaging are analytical ones such as nearest neighbor, bilinear interpolation or cubic interpolation. The multispectral debayering relies on these existing algorithms used in RGB imaging. The basic approach involves classic interpolation techniques. However, more complex methods take into account not only the information from the nearest pixel of the same channel but also the next of other channels or even further away pixels. There are many different variations of demosaicing algorithms available for RGB imaging (Malvar et al., 2004). However, implementing these algorithms for multispectral filter structures is challenging due to the different number of channels. An approach based on the weighted bilinear interpolation (Brauers and Aach, 2006) is the advancement of linear interpolation using MSFAs, called Intensity Difference (ID interpolation) (Mihoubi et al., 2015).

Further, interpolation methods based on image fusion have been proposed (Eismann and Hardie, 2005; Bendoumi et al., 2014; Zhang, 2014). Fusion based methods usually require the availability of a guiding image with higher spatial resolution, which is difficult to obtain in many scenarios.

Demosaicing by interpolation based techniques, both traditional as well as fusion-based, is easy to achieve, however, these methods suffer from color artifacts and lead to lower spatial resolution. Especially at edges, they do not take into account the spectral correlations between adjacent bands as well as due to crosstalk. This results in spectral distortions in the demosaiced image, especially for increasing mosaic filter size.

Alternatively, deep neural networks can be trained to account for scene information as well as correlations between individual spectral bands.

2.1 Network-Based Demosaicing

Demosaicing using convolutional neural networks (CNN) was first proposed for images with 2×2 Bayer pattern (Wang, 2014; Gharbi et al., 2016). In recent years, CNN based color image super resolution (SR) has gained popularity. Examples of such networks include SRCNN (Dong et al., 2014), DCSCN (Yamanaka et al., 2017) and EDSR (Lim et al., 2017). Due to their success, these networks have been extended to HSI super resolution (Li et al., 2018). The underlining aspect of all CNN based HSI demosaicing networks is the utilization of spatial and spectral context from the data during training.

Nevertheless there is only a small number of publications where CNNs are used for patterns $> 2 \times 2$. In the NTIRE 2022 Spectral Demosaicing Challange several deep learning-based demosaicing algorithms were introduced (Arad et al., 2022b). The leading methods all involved very large and complex network structures, such as an enhanced HAN (Niu et al., 2020), NLRAN and a Res2-Unet (Song et al., 2022) based method. An interesting approach for the reconstruction of MSI uses leaner network structures of five residual blocks (Shinoda et al., 2018). Bilinear interpolated data are used as input for this refinement approach. Furthermore, there are already approaches to replace the bilinear interpolation by the ID interpolation (Göb et al., 2021). Dijkstra et al. (2019) proposed a similarity maximization network for HSI demosaicing, inspired by single image SR. This network learns to reconstruct a downsampled HSI by upscaling via deconvolutional layers. The network results are presented for a 4×4 mosaic pattern and the demosaiced HSI showed high spatial and spectral resolution. Habtegebrial et al. (2019) used residual blocks to learn the mapping between low and high resolution HSI, inspired by the HCNN+ architecture (Shi et al., 2018). These two networks use 2D convolutions in order to learn the spectral-spatial correlations. An important characteristic of HSI is the correlation between adjacent spectral bands which are not taken into account when using 2D convolutional based networks. These correlations can be incorporated by using 3D convolutional networks. Mei et al. (2017) proposed one of the first 3D CNNs for hyperspectral image SR addressing both the spatial context between neighboring pixels as well as the spectral correlation between adjacent bands of the image. A more effective way to learn the spatial and spectral correlations is through a mixed 2D/3D convolutional network (Li et al., 2020).

Further, deep learning (DL) have been employed in order to predict HSI data from MSI or even classic RGB image data (Arad et al., 2022a, 2020). However, the main problem here is the lack of training data and the large dependence of the method on the application and training data. This means that the spectral behavior of individual scenes is learned by the DL model for interpolation and thus there is a dependency between the planned application and training data, which can lead to poor results and incorrect hyperspectral data if the training data is improperly selected, of poor quality, or too small in scope (Wang et al., 2021). Thus, the need of high quality ground truth data is essential. In such a dataset, each pixel should contain the entire spectral information, which is difficult to acquire in a natural environment.

2.2 Datasets

In order to be able to train and evaluate networks, both fully completed data cubes and the corresponding raw data are required. For this purpose, a number of different databases containing are available. One major challenge for the task of snapshot mosaic HSI demosaicing using neural networks is the lack of real world ground truth data.

The only databases available are those that use either the pushbroom method or spatio-spectral-line scans, usually realized by a liquid crystal. Hence, the data has different characteristics than snapshot mosaic data (e.g., missing cross-talk) and therefore a trained network cannot adequately represent reality. However, we are not aware of any data sets that include MSFAs. All HSI databases used in this work are presented in Tab. 1 and include a large number of different colored objects.

One alternative to include real MSFA data into training is to downsample captured snapshot mosaic data as presented in Dijkstra et al. (2019). However, simple downsampling leads to differences in distances of adjacent pixels, which affects the network results in an unknown manner. Therefore, this approach is not been followed in this work.

3 NETWORK ARCHITECTURE

In the following, three different architecture types are presented. All are based on different works recently published and have been modified in order to achieve improved demosaicing results.

3.1 **ResNet-Based Architecture**

In the initial phase, we aimed to enhance the network proposed by Shinoda et al. (2018). The modifications can be classified into two components: the preprocessing of input data and the CNN itself. Due to its superior effectiveness, we use ID interpolation as input of the network.

The alterations made to the CNN were intended to reduce the number of parameters without compromising the quality and are visualized in Fig. 2. Initially, the network comprised of five residual blocks. The first two blocks contained two *conv*-blocks in the main-path and one *conv*-block in the skip-connection, while the next three residual blocks consisted of three *conv*-blocks in the main-path and one *conv*-block in the skip-connection. The number of filters increased from the first to the fifth residual block with 8/16/32/64/64, and were formed by a 3D kernel-size

Dataset	# Images	Size [px]	Spectrum [nm]	Bands	Range
CAVE (Yasuma et al., 2010)	32	512x512	400-700	31	1:65536
HyTexiLa (Khan et al., 2018)	112	1024x1024	405-996	186	0:1
TokyoTech31 (Monno et al., 2015)	30	500x500	420-720	31	0:1
TokyoTech59 (Monno et al., 2018)	16	512x512	420-1000	59	0:1
SIDRI-v10 (Mirhashemi, 2019)	5	640x480	400-1000	121	0:1
SIDRI-vis (Mirhashemi, 2019)	1	640x480	400-720	31	0:1
ODSI-DB Nuance (Hyttinen et al., 2020)	139	1392x1040	450-950	51	1:65536
ODSI-DB Specim (Hyttinen et al., 2020)	171	Various	400-1000	204	1:65536
Google	670	480x1312	400-1000	396	1:4096
	1				

Table 1: The used hyperspectral data collections.

Table 2: The number of parameters and sizes of the input images of the different networks. If two input sizes are stated, the network structure needs different input.

Network	Parameter	Input Size
ID-ResNet-L	697k	$[16 \times 100 \times 100]$
ID-ResNet-S	118k	$[16 \times 100 \times 100]$
ID-UNet	128k	$\begin{bmatrix} 16 \times 100 \times 100 \\ [1 \times 100 \times 100] \end{bmatrix}$
Parallel-S	331k	$[16 \times 100 \times 100] \\ [1 \times 100 \times 100]$
Parallel-L	382k	$ \begin{bmatrix} 16 \times 25 \times 25 \\ [1 \times 100 \times 100] \end{bmatrix} $
UNet	227k	$[1 \times 100 \times 100]$
ResNet (Shinoda et al., 2018)	697k	$[16 \times 100 \times 100]$
Parallel (Wisotzky et al., 2022)	281k	$\begin{bmatrix} 16 \times 25 \times 25 \\ 1 \times 100 \times 100 \end{bmatrix}$
initial initia i initia	<i>N=64</i>	N=64 Ieun
		Conv 3x3x3, ReLU Conv 1x1x1, ReLU
intesting N=10	demosatcing	Conv 1x1x1 ResNet Block with N filters per conv Block ResNet Shinoda ResNet Small

Figure 2: The ResNet-based architectures. Top: ResNet according to Shinoda et al. (2018). Bottom: our modified version.

of $3 \times 3 \times 3$. Since our data input shows improved quality, we optimize the architecture by reducing the number of residual blocks to two. To achieve the desired quality of the CNN, we modified the number of *conv*-blocks to four in the main-path and one in the skip-connection, with 16 filters in the first residual block and 32 in the second. These modifications reduced the overall number of parameters presented in Tab. 2.

3.2 U-Net-Based Architecture

Originally introduced for medical image segmentation, the U-Net is a classical approach to reconstruct images (Ronneberger et al., 2015). Specifically, the downsampling path of the U-Net captures the context of the image, while the upsampling path performs the complete reconstruction. To transfer information from the downsampling path to the upsampling path, skip connections are used. In this work, we modified the skip connections to insert external information for reconstruction improvements. We utilize a fully reconstructed image obtained by classical demosaicing, i.e., ID interpolation, which is then inserted into the upsampling path via the skip connection. A detailed schematic of this approach is provided in Fig. 3.



Figure 3: The U-Net-based architecture. A small U-Net structure is used, while instead of the skip connection, we insert the results from ID interpolation in the network.

The input to the U-Net is the 2D MSFA. To ensure a small, simple, and effective network architecture, we limit the downsampling layer to a max-pool $4 \times 4 \times 1$ operation and reconstruct the image in its 16 spectral regions using a $4 \times 4 \times 16$ kernel in the upsampling path. The *conv*-blocks in the network consist of 16 filters in the upper layers and 32 filters in the lower layers and are provided with $3 \times 3 \times 3$ kernels.

3.3 Parallel Architecture

As third, we use a CNN architecture with parallel building blocks to reconstruct the correct spatialspectral distribution in the image. We elaborated two general types based on literature (Dijkstra et al., 2019; Shinoda et al., 2018; Habtegebrial et al., 2019; Wisotzky et al., 2022). First, two parallel feature extracting layers using a mosaic to cube converter (M2C) on one side and ResNet blocks on the other side are used followed by a feature adding and two deconvolution (*deconv*) layers to upsample the spatial dimensions of the image. The second implementation combines two effective approaches introduced by Dijkstra et al. (2019) and Shinoda et al. (2018)/Habtegebrial et al. (2019), which are added and refined to form the demosaiced output. Both implementations use 3D kernels and are presented in Fig. 4.



Figure 4: The parallel CNN architectures. Top: network Parallel-L is an extension of Wisotzky et al. (2022) using the small ResNet-structure (cf. Fig. 2). Bottom: network Parallel-S is a combination of two effective approaches.

4 DATA AND TRAINING

During training, we used image patches of size $[1 \times 100 \times 100]$ (representing the mosaic sensor output) as input for the network. The output and ground truth data had a size of $[16 \times 100 \times 100]$. Depending on the model, the input is either left unchanged or was transformed in the following way:

- Transformation to a sparse 3D cube where empty values are filled with mean; size: $[16 \times 100 \times 100]$
- Transformation to a 3D cube with low resolution and smaller spatial size; size: $[16 \times 25 \times 25]$
- Transformation to a 3D cube by ID interpolation; size: $[16 \times 100 \times 100]$.

On each side of the images, we removed four pixels resulting in a shape of 92×92 px, because ID interpolation distorts those outermost pixels making it more difficult for the models to predict the correct interpolation.

In order to train and validate the networks proposed in this work, a large HSI data set was built from different data collections introduced earlier. To allow comparability between the individual data collections, the value range of all HSI data are normalized to [0, 1]. The data set was split into 75% training, 15% validation and 10% test data. As described, the data does not represent real snapshot mosaic behavior including cross-talk and characteristic filter responses for each mosaic pixel. Therefore, an MSFA had to be simulated. First, we just selected 16 wavelengths in the range of 450 – 630 nm, interpolated these bands from the HSI data and built an MSFA as widely been done in literature (Arad et al., 2020, 2022a; Göb et al., 2021; Habtegebrial et al., 2019). We refer to this data set as *SimpleData*.

In addition, we built a data set better representing real captured MSFAs by transforming the stated reflectances of the data $r(\lambda)$ into real MSI snapshot camera measurements r_b at band b according to

$$r_b = \frac{\int_{\lambda_{\min}}^{\lambda_{\max}} T(\lambda) I(\lambda) f_b(\lambda) r(\lambda) d\lambda}{\int_{\lambda_{\min}}^{\lambda_{\max}} T(\lambda) I(\lambda) f_b(\lambda) d\lambda},$$
 (1)

where T is the optical transmission profile of the optical components of our used hardware setup, f_b characterize the optical filter responses of each of the b spectral bands of the used camera (Mühle et al., 2021; Wisotzky et al., 2020), and I is the relative irradiance of the light source. All profiles are well known and allow to transform HSI data into real MSI snapshot camera outputs. We refer to this data set as *SimRealData*.

For training, we used the ADAM optimizer with an adaptive learning rate strategy and an initial learning rate of 0.0002. At every 10th epoch, the learning rate is reduced by the factor 0.9. We trained each model for 100 epochs. The batch size was 20. The loss function for calculating the difference between the ground truth and the predicted full-spectrum hyperspectral cube is defined by the mean squared error (MSE)

$$MSE(o,p) = \frac{1}{N} \sum_{i=0}^{N} |o_i - p_i|^2, \qquad (2)$$

where o is the ground truth and p is the predicted value. To evaluate model performance, we calculated the structural similarity index (SSIM), peak signal-to-noise ratio (PSNR) and spectral angle mapper (SAM).

5 RESULTS AND DISCUSSION

In the following, we present the evaluation results of the predictions of our presented network architectures. For this purpose, they are examined and compared in a quantitative and qualitative manner. We compare our proposed networks with classical interpolation approaches, bilinear and ID interpolation, as well as with different reference network approaches introduced in Sec. 2: ResNet (Shinoda et al., 2018), HSUp (Dijkstra et al., 2019), U-Net and Parallel (Wisotzky et al., 2022).

Further, we analyze the resulting images visually and, to show the usability of our work, we visually analyze intraoperative snapshot images acquired during a surgery of parotidectomy.

5.1 Quantitative Results

All networks, our proposed networks as well as the different references, were trained on the two created datasets *SimpleData* and *SimRealData*. For both dataset modifications, the networks learned to predict a full spectral cube of dimension $[16 \times 100 \times 100]$ from the given input images. Our networks outperformed or were in the same range as the reference networks for both datasets.

5.1.1 SimpleData

For the SimpleData without cross-talk all modified and newly introduced networks perform better that the state-of-the-art methods, see Tab. 3. The large modified ResNet-based model using ID interpolation as input performed significantly best. The larger the network in terms of trainable parameter the better the results for all three evaluation measures, but also the slower the network performance. In comparison with the reference ResNet model (Shinoda et al., 2018), the quality of the input image, i.e., the quality of the initial demosaicing, is of high relevance. Using better input quality (ID instead of bilinear interpolation), the ResNet is able to achieve an relatively higher increases in reconstruction accuracy. It can be assumed that with even better initial demosaiced data by using network-based demosaicing methods, the perfor-

Table 3: Demosaicing results on *SimpleData* patches. Best result is bold, second best is bold-italic and third rank is italic.

Network	SSIM	PSNR [dB]	SAM
ID-ResNet-L	0.9891	52.3846	3.48e-02
ID-ResNet-S	0.9856	51.1377	3.90e-02
ID-UNet	0.9868	51.3331	3.85e-02
Parallel-S	0.9865	51.4654	3.78e-02
Parallel-L	0.9857	51.1386	3.93e-02
UNet	0.9839	50.5408	4.25e-02
ResNet	0.9792	48.9982	4.07e-02
Parallel	0.9863	51.1316	3.96e-02
HSUp	0.9846	50.8835	4.05e-02
Bilinear	0.9235	37.5282	5.90e-02
ID	0.9671	39.7182	5.27e-02

mance is further improved. However, this would also increase the number of parameters and thus reduce performance.

The network Parallel-S follows the ID-ResNet-L model in reconstruction accuracy. It performed as second best in PSNR and SAM metrics and third in SSIM. The performance order is switched with the ID-UNet, which is third in PSNR and SAM, and second in SSIM. The Parallel-L network, which includes the smaller ID-ResNet-S, shows an improvement in comparision to ID-ResNet-S. Both methods are fourth and fifth in terms of the analyzed metrics. Thus, all proposed methods and modifided networks performing better than the compared modalities from literature. This also shows that it is possible to greatly reduce the network complexity (by up to six times: 118k network parameters for ID-ResNet-S instead of 697k parameters for ID-ResNet-L) with only minor loss of quality compared to the best performing model.

Interestingly, also with respect to other recent work (Arad et al., 2022b), it appears that the complexity of the models, i.e., the number of model paramter, has a great impact on the quality of the demosaicing results on simple, rather unrealistic, data sets. Because after all, the best results in this study are also achieved with the most complex models.

5.1.2 SimRealData

For the *SimRealData*, which much better represent real captured data, the results of all networks, proposed as well as reference networks, are very much improved in comparison to *SimpleData*, see Tab. 4. Further, the difference between the reconstruction results of all networks is reduced. Again the largest network ID-ResNet-L performed best, but closely followed by the parallel networks. Interestingly, the state-of-the-art parallel model is performing second best, closely followed by Parallel-S. The other networks, expect for the standard U-Net, are following closely. Thus, networks with only 40% or 50% of the parameters (Parallel or Parallel-S, respectively)

Table 4: Demosaicing results on *SimRealData*. Best result is bold, second best is bold-italic and third rank is italic.

Network	SSIM	PSNR	SAM
ID-ResNet-L	0.9989	62.0690	1.29e-02
ID-ResNet-S	0.9984	60.6000	1.55e-02
ID-UNet	0.9985	60.7327	1.58e-02
Parallel-S	0.9983	60.9021	1.44e-02
Parallel-L	0.9982	60.5968	1.52e-02
UNet	0.9973	58.3865	2.28e-02
Parallel	0.9986	61.2197	1.41e-02
HSUp	0.9983	60.6398	1.50e-02



Figure 5: Visual results and error images. Spectral data are represented in RGB and error images of two region of interest (ROI) are build using l_1 -Norm. The maximum errors in the top ROI are 0.0598, 0.0994, 0.1001, 0.0805, 0.0667 and in the bottom ROI are 0.0401, 0.0597, 0.0614, 0.0520, 0.0366 in order of appearance of the models from left to right.

achieve similarly good reconstruction results.

Obviously, the complexity of the networks is not decisive for the reconstruction results, but rather the quality of the input data and the general structure. The networks can draw information about all spectral bands from the complex spectral behavior of the individual pixels on an MSFA. The effect of cross-talk contains essential data, which are useful to all networks for a more precise spectral interpolation. This allows using simpler network structures while maintaining similar high reconstruction quality.

5.2 Qualitative Results

An analysis of the individual spectral channels did not reveal any discernible deviations in the quality characteristics between the spectral channels. Thus, no channel stands out as particularly defective during the demosaicing process. Therefore, the qualitative analysis of the results is made on RGB-calculated images.

As can be seen in Fig. 5, all reconstruction results appear in similar quality at first glance. On closer inspection, minor differences are evident at strong image edges, e.g., at the bottom right wing. These small differences can be quantitatively represented in a difference image (Fig. 5) or in a spectral plot, Fig. 6.

In addition, we have demosaiced intraoperative images, see Fig. 7. In terms of quality, these im-



Figure 6: Spectral plot of a central left point in the left top wing of the butterfly in Fig. 5. The SAM of the spectra in comparison to the ground truth are 0.0133, 0.0157, 0.0158, 0.0265, 0.0276 for the models ID-Resnet-L, Parallel-S, Parallel-L, ID-UNet and ID-Resnet-S, respectively.

ages show a high resolution as small details as well as edges are clearly visible. It is also noticeable that artifacts such as color fringes are reduced.

6 CONCLUSION

In conclusion, our results clearly show that significant improvements in demosaicing algorithms can be achieved by using well-designed neural network architectures. The networks and modifications we have introduced feature excellent reconstruction of the ground truth data while reducing or at least hold-



Figure 7: Demosaiced medical image showing qualitatively high image quality.

ing the model parameters constant. The results were tested both quantitatively and qualitatively, showing convincing results over traditional as well as CNNbased demosaicing methods.

Due to comparatively fewer network parameter, our networks result in more efficient computation proving the capability for real-time application, e.g., for intraoperative hyperspectral image application. Especially in comparison to current work (Arad et al., 2022b), which uses very complex networks and achieves similar results, this is a gain. Importantly, our focus is on correct spectral reconstruction rather than visual attractiveness, which is of high importance for the mentioned applications and supported by the quantitative results confirmed by our qualitative evaluation.

Moreover, the differences between the results of different datasets, in agreement with the existing literature Dijkstra et al. (2019), provide valuable insights for the demosaicing of real camera data. This underscores the importance of developing demosaicing solutions that train on data being as close as possible to real MSFA data. Our results demonstrated that the use of synthetic representatives of real MSFA data are suitable for training and networks trained on these data perform well despite fewer training parameters, thereby enabling fast processing. This pursuit of efficient solutions is critical for practical applications in various fields, including medical imaging and remote sensing, allowing to integrate compact acquisition concepts like snapshot mosaic imaging into such processes.

ACKNOWLEDGMENT

This work was funded by the German Federal Ministry for Economic Affairs and Climate Action

(BMWK) under Grant No. 01MK21003 (NaLamKI). Only tissue that has been exposed during normal surgical treatment has been scanned additionally with our described camera. This procedure has been approved by Charité–Universitätsmedizin Berlin, Germany.

REFERENCES

- Arad, B., Timofte, R., Ben-Shahar, O., Lin, Y.-T., and Finlayson, G. D. (2020). Ntire 2020 challenge on spectral reconstruction from an rgb image. In *Proceedings of* the IEEE/CVF Conference on Computer Vision and Pattern Recognition (CVPR) Workshops.
- Arad, B., Timofte, R., Yahel, R., Morag, N., Bernat, A., Cai, Y., Lin, J., Lin, Z., Wang, H., Zhang, Y., Pfister, H., Van Gool, L., Liu, S., Li, Y., Feng, C., Lei, L., Li, J., Du, S., Wu, C., Leng, Y., Song, R., Zhang, M., Song, C., Zhao, S., Lang, Z., Wei, W., Zhang, L., Dian, R., Shan, T., Guo, A., Feng, C., Liu, J., Agarla, M., Bianco, S., Buzzelli, M., Celona, L., Schettini, R., He, J., Xiao, Y., Xiao, J., Yuan, Q., Li, J., Zhang, L., Kwon, T., Ryu, D., Bae, H., Yang, H.-H., Chang, H.-E., Huang, Z.-K., Chen, W.-T., Kuo, S.-Y., Chen, J., Li, H., Liu, S., Sabarinathan, S., Uma, K., Bama, B. S., and Roomi, S. M. M. (2022a). Ntire 2022 spectral recovery challenge and data set. In 2022 IEEE/CVF Conference on Computer Vision and Pattern Recognition Workshops (CVPRW), pages 862-880.
- Arad, B., Timofte, R., Yahel, R., Morag, N., Bernat, A., Wu, Y., Wu, X., Fan, Z., Xia, C., Zhang, F., Liu, S., Li, Y., Feng, C., Lei, L., Zhang, M., Feng, K., Zhang, X., Yao, J., Zhao, Y., Ma, S., He, F., Dong, Y., Yu, S., Qiu, D., Liu, J., Bi, M., Song, B., Sun, W., Zheng, J., Zhao, B., Cao, Y., Yang, J., Cao, Y., Kong, X., Yu, J., Xue, Y., and Xie, Z. (2022b). Ntire 2022 spectral demosaicing challenge and data set. In *Proceedings* of the IEEE/CVF Conference on Computer Vision and Pattern Recognition, pages 882–896.
- Bendoumi, M. A., He, M., and Mei, S. (2014). Hyperspectral image resolution enhancement using highresolution multispectral image based on spectral unmixing. *IEEE Transactions on Geoscience and Remote Sensing*, 52(10):6574–6583.
- Brauers, J. and Aach, T. (2006). A color filter array based multispectral camera. In 12. Workshop Farbbildverarbeitung, pages 5–6. Ilmenau.
- Calin, M. A., Parasca, S. V., Savastru, D., and Manea, D. (2014). Hyperspectral imaging in the medical field: present and future. *Applied Spectroscopy Reviews*, 49(6):435–447.
- Dijkstra, K., van de Loosdrecht, J., Schomaker, L., and Wiering, M. A. (2019). Hyperspectral demosaicking and crosstalk correction using deep learning. *Machine Vision and Applications*, 30(1):1–21.
- Dong, C., Loy, C. C., He, K., and Tang, X. (2014). Learning a deep convolutional network for image super-

resolution. In *European conference on computer vision*, pages 184–199. Springer.

- Eismann, M. T. and Hardie, R. C. (2005). Hyperspectral resolution enhancement using high-resolution multispectral imagery with arbitrary response functions. *IEEE Transactions on Geoscience and Remote Sensing*, 43(3):455–465.
- Gharbi, M., Chaurasia, G., Paris, S., and Durand, F. (2016). Deep joint demosaicking and denoising. ACM Transactions on Graphics (TOG), 35(6):1–12.
- Göb, S., Götz, T. I., and Wittenberg, T. (2021). Multispectral single chip reconstruction using dnns with application to open neurosurgery. *Current Directions in Biomedical Engineering*, 7(2):37–40.
- Habtegebrial, T. A., Reis, G., and Stricker, D. (2019). Deep convolutional networks for snapshot hypercpectral demosaicking. In 2019 10th Workshop on Hyperspectral Imaging and Signal Processing: Evolution in Remote Sensing (WHISPERS), pages 1–5. IEEE.
- Hershey, J. and Zhang, Z. (2008). Multispectral digital camera employing both visible light and non-visible light sensing on a single image sensor. US Patent 7,460,160.
- Hyttinen, J., Fält, P., Jäsberg, H., Kullaa, A., and Hauta-Kasari, M. (2020). Oral and dental spectral image database—odsi-db. *Applied Sciences*, 10(20):7246.
- Jung, A., Kardeván, P., and Tőkei, L. (2006). Hyperspectral technology in vegetation analysis. *Progress in Agricultural Engineering Sciences*, 2(1):95–117.
- Khan, H. A., Mihoubi, S., Mathon, B., Thomas, J.-B., and Hardeberg, J. Y. (2018). Hytexila: High resolution visible and near infrared hyperspectral texture images. *Sensors*, 18(7):2045.
- Li, Q., Wang, Q., and Li, X. (2020). Mixed 2d/3d convolutional network for hyperspectral image superresolution. *Remote Sensing*, 12(10):1660.
- Li, Y., Zhang, L., Dingl, C., Wei, W., and Zhang, Y. (2018). Single hyperspectral image super-resolution with grouped deep recursive residual network. In 2018 IEEE Fourth International Conference on Multimedia Big Data (BigMM), pages 1–4. IEEE.
- Lim, B., Son, S., Kim, H., Nah, S., and Mu Lee, K. (2017). Enhanced deep residual networks for single image super-resolution. In *Proceedings of the IEEE conference on computer vision and pattern recognition workshops*, pages 136–144.
- Lu, G. and Fei, B. (2014). Medical hyperspectral imaging: a review. *Journal of Biomedical Optics*, 19(1):10901.
- Malvar, H. S., He, L.-w., and Cutler, R. (2004). Highquality linear interpolation for demosaicing of bayerpatterned color images. In 2004 IEEE International Conference on Acoustics, Speech, and Signal Processing, volume 3, pages iii–485. IEEE.
- Mei, S., Yuan, X., Ji, J., Zhang, Y., Wan, S., and Du, Q. (2017). Hyperspectral image spatial super-resolution via 3d full convolutional neural network. *Remote Sensing*, 9(11):1139.
- Mihoubi, S., Losson, O., Mathon, B., and Macaire, L. (2015). Multispectral demosaicing using intensitybased spectral correlation. In *International Confer-*

ence on Image Processing Theory, Tools and Applications (IPTA), volume 5, pages 461–466. IEEE.

- Mirhashemi, A. (2019). Configuration and registration of multi-camera spectral image database of icon paint-ings. *Computation*, 7(3):47.
- Moghadam, P., Ward, D., Goan, E., Jayawardena, S., Sikka, P., and Hernandez, E. (2017). Plant disease detection using hyperspectral imaging. In 2017 International Conference on Digital Image Computing: Techniques and Applications (DICTA), pages 1–8. IEEE.
- Monno, Y., Kikuchi, S., Tanaka, M., and Okutomi, M. (2015). A practical one-shot multispectral imaging system using a single image sensor. *IEEE Transactions on Image Processing*, 24(10):3048–3059.
- Monno, Y., Teranaka, H., Yoshizaki, K., Tanaka, M., and Okutomi, M. (2018). Single-sensor rgb-nir imaging: High-quality system design and prototype implementation. *IEEE Sensors Journal*, 19(2):497–507.
- Mühle, R., Markgraf, W., Hilsmann, A., Malberg, H., Eisert, P., and Wisotzky, E. L. (2021). Comparison of different spectral cameras for image-guided organ transplantation. *Journal of Biomedical Optics*, 26(7):076007.
- Niu, B., Wen, W., Ren, W., Zhang, X., Yang, L., Wang, S., Zhang, K., Cao, X., and Shen, H. (2020). Single image super-resolution via a holistic attention network. In *Computer Vision–ECCV 2020: 16th European Conference, Glasgow, UK, August 23–28, 2020, Proceedings, Part XII 16*, pages 191–207. Springer.
- Ronneberger, O., Fischer, P., and Brox, T. (2015). Unet: Convolutional networks for biomedical image segmentation. In Medical Image Computing and Computer-Assisted Intervention–MICCAI 2015: 18th International Conference, Munich, Germany, October 5-9, 2015, Proceedings, Part III 18, pages 234–241. Springer.
- Shafri, H. Z., Taherzadeh, E., Mansor, S., and Ashurov, R. (2012). Hyperspectral remote sensing of urban areas: an overview of techniques and applications. *Research Journal of Applied Sciences, Engineering and Technology*, 4(11):1557–1565.
- Shi, Z., Chen, C., Xiong, Z., Liu, D., and Wu, F. (2018). Hscnn+: Advanced cnn-based hyperspectral recovery from rgb images. In *Proceedings of the IEEE Conference on Computer Vision and Pattern Recognition Workshops*, pages 939–947.
- Shinoda, K., Yoshiba, S., and Hasegawa, M. (2018). Deep demosaicking for multispectral filter arrays. arXiv preprint arXiv:1808.08021.
- Song, B., Ma, S., He, F., and Sun, W. (2022). Hyperspectral reconstruction from rgb images based on res2-unet deep learning network. *Opt Precis Eng*, 30(13):1606.
- Wang, Y., Cao, R., Guan, Y., Liu, T., and Yu, Z. (2021). A deep survey in the applications of demosaicking. In 2021 3rd International Academic Exchange Conference on Science and Technology Innovation (IAECST), pages 596–602. IEEE.
- Wang, Y.-Q. (2014). A multilayer neural network for image demosaicking. In 2014 IEEE International Confer-

VISAPP 2024 - 19th International Conference on Computer Vision Theory and Applications

ence on Image Processing (ICIP), pages 1852–1856. IEEE.

- Wisotzky, E. L., Daudkane, C., Hilsmann, A., and Eisert, P. (2022). Hyperspectral demosaicing of snapshot camera images using deep learning. In *DAGM German Conference on Pattern Recognition*, pages 198–212. Springer.
- Wisotzky, E. L., Kossack, B., Uecker, F. C., Arens, P., Hilsmann, A., and Eisert, P. (2020). Validation of two techniques for intraoperative hyperspectral human tissue determination. *Journal of Medical Imaging*, 7(6).
- Wisotzky, E. L., Uecker, F. C., Arens, P., Dommerich, S., Hilsmann, A., and Eisert, P. (2018). Intraoperative hyperspectral determination of human tissue properties. *Journal of Biomedical Optics*, 23(9):1–8.
- Yamanaka, J., Kuwashima, S., and Kurita, T. (2017). Fast and accurate image super resolution by deep cnn with skip connection and network in network. In *International Conference on Neural Information Processing*, pages 217–225. Springer.
- Yasuma, F., Mitsunaga, T., Iso, D., and Nayar, S. K. (2010). Generalized assorted pixel camera: postcapture control of resolution, dynamic range, and spectrum. *IEEE transactions on image processing*, 19(9):2241–2253.
- Zhang, Y. (2014). Spatial resolution enhancement of hyperspectral image based on the combination of spectral mixing model and observation model. In *Image and Signal Processing for Remote Sensing XX*, volume 9244, page 924405. International Society for Optics and Photonics.
- Zhang, Y., Wirkert, S. J., Iszatt, J., Kenngott, H., Wagner, M., Mayer, B., Stock, C., Clancy, N. T., Elson, D. S., and Maier-Hein, L. (2017). Tissue classification for laparoscopic image understanding based on multispectral texture analysis. *Journal of Medical Imaging*, 4(1):015001–015001.