# GAN-Based Data Augmentation for Improving Biometric Authentication Using CWT Images of Blood Flow Sounds

Natasha Sahare<sup>1,2</sup>, Patricio Fuentealba<sup>3</sup><sup>®</sup>, Rutuja Salvi<sup>4</sup>, Anja Burmann<sup>1</sup><sup>®</sup> and Jasmin Henze<sup>1</sup><sup>©</sup>

<sup>1</sup>Fraunhofer Institute for Software and Systems Engineering ISST, Dortmund, Germany
<sup>2</sup>Technical University of Dortmund, Dortmund, Germany
<sup>3</sup>Instituto de Electricidad y Electrónica, Facultad de Ciencias de la Ingeniería,

Universidad Austral de Chile, Valdivia, Chile <sup>4</sup>IDTM GmbH, Recklinghausen, Germany

Keywords: Data Augmentation, Generative Adversarial Networks, Continuous Wavelet Transform, Convolutional Neural Networks, Blood Flow Sounds, Biometry.

Abstract: Biometric identification allows to secure sensitive information. Since existing biometric traits, such as fingerprings, voice, etc. are associated with different limitations, we exemplified the potential of blood flow sounds for biometric authentication in previous work. Therefore, we used measurements from seven different users acquired with a custom-built auscultation device to calculate the spectrograms of these signals for each cardiac cycle using continuous wavelet transform (CWT). The resulting spectral images were then used for training of a convolutional neural network (CNN). In this work, we repeated the same experiment with data from twelve users by adding more data from the original seven users and data from five more users. This lead to an imbalanced dataset, where the amount of available data for the new users was much smaller, e.g., U1 had more than 900 samples per side whereas the new user U9 had less than 100 samples per side. We experienced a lower performance for the new users, i.e. their sensitivity was 18-21% lower than the overall accuracy. Thus, we examined whether the augmentation of data leads to better results. This analysis was performed using generative adversarial networks (GANs). The newly generated data was then used for training of a CNN with several different settings, revealing the potential of GAN-based data augmentation for increasing the accuracy of biometric authentication using blood flow sounds.

# **1 INTRODUCTION**

Biometric identification systems are used to provide security to data, as biometric data of an individual is unique (Babiker et al., 2017). Existing biometric traits, such as fingerprints, voice, face, iris, gait, signature and handwriting are associated with several limitations and drawbacks including susceptibility to forgery, lifelong persistence issues and sensitivity to external environmental conditions. The search for alternative biometric characteristics led to the discovery of electrocardiogram (ECG) signals and heart sounds, which offer novel biometric information. While ECG signals present unique advantages such as resistance to tampering and forging, they require a complex setup with electrodes and are relied on electronic stethoscope for heart sound recordings. The exploration of these biological characteristics aims to overcome the shortcomings of traditional biometric methods and enhance the reliability of biometric sensing tools. (Salvi and et al., 2021b)

In previous works, we demonstrated the potential of blood flow sounds from the carotid arteries, acquired by a custom-built auscultation device, for person identification (Salvi and et al., 2021b), (Henze and et al., 2022). Therefore, we analysed the sound signals in the frequency domain using continuous wavelet transform (CWT), assuming that the spectral energies in the blood flow sound contain significant information for the identification of an individual. We then trained two simple Convolutional Neural Networks (CNN) on the CWT images from those mea-

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Sahare, N., Fuentealba, P., Salvi, R., Burmann, A. and Henze, J.

GAN-Based Data Augmentation for Improving Biometric Authentication Using CWT Images of Blood Flow Sounds. DOI: 10.5220/0012318100003657

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<sup>&</sup>lt;sup>a</sup> https://orcid.org/0000-0002-7119-0580

<sup>&</sup>lt;sup>b</sup> https://orcid.org/0000-0002-6989-1230

<sup>&</sup>lt;sup>c</sup> https://orcid.org/0000-0001-7180-2578

In Proceedings of the 17th International Joint Conference on Biomedical Engineering Systems and Technologies (BIOSTEC 2024) - Volume 2, pages 340-345 ISBN: 978-989-758-688-0; ISSN: 2184-4305

surements, separately for measurements from each side. Therefore, we chose each heart cycle within the measurements as a single sample for training and testing. Irrespective of the side on which the measurements were taken, this approach achieved an overall accuracy of over 95% for identifying 881 samples from seven users. The confusion matrices for the experiments on both sides are shown in Figure 1. As can be seen, the sensitivities for each single user (marked in dark blue) vary between 0.91 and 0.97 for the experiment on the left side data and between 0.94 and 0.97 on the right side data.

In this work, we add more measurements from the same seven users but also from five additional users to further investigate the potential of blood flow sounds for biometric authentication, leading to a dataset of 1,765 samples in total. With retraining the CNN on the new dataset, it achieves an overall accuracy of over 87% with sensitivity values of over 90% for most users. However, it clearly drops for users that contributed with fewer samples to the dataset. Thus, we investigate data augmentation techniques such as generative adversarial networks (GANs) and conditional adversarial networks (CGANs) to research whether the model's accuracy enhances by adding synthetic data to the real data.

As a first step, we generate synthetic images using both approaches and compare the results on a small subset of three users. An investigation using the Fréchet inception distances (FID) shows that the images generated by the GANs are more similar to the original images and have smaller FID than the ones generated by the CGAN. Matching that, the classification results using the GANs-generated samples are slightly better than those using the CGAN-generated samples. However, training of a separate GAN for each of the labels takes significantly longer than training one CGAN for all labels. Since the improvement in classification is very small, we therefore continue the experiments on the whole dataset with the CGAN. Strategic use of 30% CGAN-generated data and 70% real data yields the best results, improving sensitivity for all users and specific labels by 6-10%. This study highlights the trade-off between reliability and training time for GANs and CGANs and shows the potential benefits of synthetic data augmentation in limited data domains.

## 2 MATERIAL AND METHODS

# 2.1 Data

The employed data includes 1,765 carotid sound recordings sampled at 16 kHz acquired by a custombuilt audio auscultation device (Salvi and et al., 2021a), (Sühn and et al., 2020). Each recording consists of 11 s in length and was collected between December 2020 and April 2022 from twelve users (U1-U12). As shown in Table 1, the number of signals acquired from the left and right carotid arteries are overall balanced. They are analysed independently for each side.



Figure 1: Confusion matrices from previous experiments showing the results from CNNs trained on blood flow sounds from seven people for differentiation between the individuals. Separately trained on data from the left side (top) and right side (bottom). Sensitivities for each single user are shown on the diagonal.

All signals were recorded under controlled cessation of breathing (apnea) to avoid potential noise generated from breathing episodes. To evaluate the signal quality, we visually examined the presence of S1 and S2 episodes, the main sounds produced from the mechanical contraction (systole) and relaxation (diastole) of the ventricles. As a result of this evaluation, we included 1,674 signals considered as good quality into further processing.

Table 1: Number of CWT images for each user in the dataset. Includes more data for users U1-U7 that were already part of previous work and additional data for U7-U12 that were not included in previous work.

User ID	Left	Right
U1	907	921
U2	852	855
U3	965	1015
U4	1139	1149
U5	1150	1121
U6	1023	1011
U7	337	330
U8	270	270
U9	96	80
U10	181	192
U11	138	143
U12	1103	1086

#### 2.2 Data Preparation and Classification

After gathering all the signals, we used a discrete wavelet transform to automatically detect swallowing and coughing artifacts within the signal, as presented in (Fuentealba and et al., 2021). Next, we performed a spectral analysis to look at the signal properties based on CWT. The spectral dynamics for each cardiac cycle were then independently examined using the segmentation function for phonocardiogram recordings proposed by (Springer et al., 2016). This tool uses a duration-dependent logistic regression-based Hidden Markov model to pinpoint S1, systole, S2, and diastole episodes. Following the time domain segmentation of the signal, the associated CWT spectrum was segmented in accordance. Note that the completed spectral analysis included the frequency range from 0 to fs/2 = 8 kHz.

We created a CNN with three convolutional layers with max pooling followed by two fully connected layers for the categorization of the prepared CWT images. Rectified linear activation functions are applied to all levels. The CNN determines a score for each of the available classes for each input sample, and it outputs the class with the highest score in a stratified 5-fold cross-validation with 10 repetitions. The hyperparameters in this setting were: a learning rate of 0.001, a batch size of 32 and 10 training epochs. This CNN attained an overall accuracy of over 87% for all the 12 users. The same neural network has been used from the previous study with seven users (Salvi and et al., 2021b) by updating the output layer, this time with more units, as it has to return scores for 12 instead of seven users.



Figure 2: Confusion matrices from this work's experiments showing the results from CNNs trained on blood flow sounds from twelve people (including seven from previous work) for differentiation between the individuals. Separately trained on data from the left side (top) and right side (bottom). Sensitivities for each single user are shown on the diagonal. Baseline result, does not include any synthetic data.

#### 2.3 Data Augmentation

We experienced a worse performance of our classification model for twelve users, particularly for the new users who have comparatively less data than others, as shown in Table 1. The confusion matrices for the experiments on both sides are shown in Figure 2. As can be seen, the sensitivities for each single user (marked in dark blue) vary between 0.61 and 0.96 for the experiment on the left side data and between 0.66 and 0.95 on the right side data. For some of the new users, such as U9 and U11, the sensitivity is 18-21% less than the overall accuracy. These results make us conclude that the amount of data plays an important role in the accuracy of the model prediction. Rather than asking the users to record more data, we investigated data augmentation techniques.

Popular data augmentation techniques include scaling, cropping, flipping, rotating, etc. (Shorten and Khoshgoftaar, 2019). As the CWT plots the spectrograms on the time and frequency domain, the x-axis represents time, and the y-axis gives the frequency (Addison, 2018). So, flipping or rotating would completely change the values of the spectrogram. Therefore, we used generative models, which can be used to generate new examples that plausibly could have been drawn from the original dataset. Generative adversarial networks (GANs) are widely used for producing clear and discrete synthetic outputs (Goodfellow and et al., 2014).

A Generative Adversarial Network (GAN) is comprised of two key components: the generator model and the discriminator model. The generator is tasked with creating new synthetic data, while the discriminator focuses on distinguishing between actual and generated synthetic data. The efficacy of a GAN hinges on training both models concurrently. Initially, the generator produces lower-quality data, but with ongoing training, it progressively enhances its capacity to craft more realistic data. Conversely, the discriminator begins by effortlessly discerning real and synthetic data apart. As it undergoes training, it eventually reaches a point where distinguishing between real and synthetic data becomes a formidable challenge, exemplifying the intricate equilibrium achieved within the GAN framework. (Goodfellow and et al., 2014). See Figure 3 for an example of a GAN-generated sample CWT image in comparison to a real CWT image from user U2.

GANs can only generate a single labelled output at once, i.e., we have no control over which specific label will be produced by the generator. There is no mechanism for how to request a particular label from the GANs (Mirza and Osindero, 2014). To train twelve different labels of our dataset would be quite time consuming as we would have to train GANs 12 times for 12 different users. A variation of GAN called Conditional GAN (CGAN) can address this problem. It consists of an additional input layer with values of one-hot-encoded image labels. CGANS generate multilabel output at once and are much more efficient (Mirza and Osindero, 2014).

### 2.4 Evaluation of Augmented Data

We employed the standard assessment metric known as the Fréchet Inception Distance (FID) to gauge the quality of the generated images in comparison to the authentic image set. Similar to the inception score,



Figure 3: Example of a real image from user U2 from our dataset (left) and a synthetic image generated by the GAN trained on data from U2 (right).

this evaluation utilizes the inception v3 model (Borji, 2018). Specifically, the coding layer of the model, situated just before the output classification of images, captures pertinent computer vision-oriented features from input images. These activations are computed for both real and synthetic images, their mean and covariance evaluated to render a multivariate Gaussian representation. These computed values then encapsulate the activations across the real and synthetic image samples. A perfect FID score would stand at 0.0, signifying a likeness between the two image sets (Borji, 2018).

Additionally, we assessed the practicality of GANs and CGANs in our context by comparing the classification performance attained using synthetic images from both methodologies. This evaluation was conducted on a subset comprising just three users (U1, U2, and U3). Following the outcomes outlined in Section 3, we opted to proceed with CGANs for subsequent experiments.

To ascertain the optimal ratio for harnessing synthetic generated data to increase the size of training set and consequently enhance the accuracy of biometric property analysis in blood flow sounds, we trained Convolutional Neural Networks (CNNs) under varied real-to-synthetic data proportions: 1:9 (10% synthetic to 90% augmented data), 5:5, and 3:7. Additionally, we explored an approach involving augmenting the labels with fewer data instances using GAN-generated synthetic data while keeping others constant, thereby achieving a balanced image count. Refer to Section 3 and Tables 2 and 3 for detailed insights into the outcomes of these experiments.

## **3 RESULTS**

Referring to Table 4, we can see that the FID values for CGANs (considering only the left side of users' data) are roughly twice as large as those for the corresponding GANs across the three users. This shows that the images generated by the GANs are more sim-

Table 2: Sensitivities for experiments with different combinations of real and augmented data for the left side. Column "Real" contains the results from the baseline with only real data. The columns "10%", "30%" and "50%" contain the results from experiments with the corresponding amount of augmented data. "Gap" refers to the approach of only adding as much augmented data as needed to balance the data set for those users with smaller amounts of data.

User ID	Real	10%	30%	50%	Gap
U1	0.96	0.96	0.96	0.94	0.96
U2	0.88	0.89	0.89	0.86	0.91
U3	0.91	0.93	0.94	0.90	0.91
U4	0.93	0.93	0.94	0.91	0.93
U5	0.96	0.97	0.97	0.96	0.97
U6	0.94	0.96	0.96	0.93	0.94
U7	0.90	0.91	0.93	0.91	0.93
U8	0.92	0.93	0.93	0.91	0.95
U9	0.69	0.69	0.70	0.70	0.74
U10	0.81	0.82	0.85	0.82	0.86
U11	0.66	0.67	0.69	0.67	0.76
U12	0.93	0.93	0.94	0.90	0.95

Table 3: Sensitivities for experiments with different combinations of real and augmented data for the right side. Column "Real" contains the results from the baseline with only real data. The columns "10%", "30%" and "50%" contain the results from experiments with the corresponding amount of augmented data. "Gap" refers to the approach of only adding as much augmented data as needed to balance the data set for those users with smaller amounts of data.

User ID	Real	10%	30%	50%	Gap
U1	0.95	0.95	0.95	0.93	0.96
U2	0.93	0.94	0.94	0.89	0.95
U3	0.92	0.92	0.93	0.90	0.94
U4	0.94	0.94	0.94	0.91	0.94
U5	0.92	0.93	0.94	0.91	0.94
U6	0.93	0.94	0.95	0.90	0.96
U7	0.90	0.91	0.91	0.90	0.93
U8	0.92	0.93	0.93	0.91	0.95
U9	0.66	0.69	0.70	0.64	0.74
U10	0.83	0.83	0.85	0.82	0.86
U11	0.69	0.70	0.72	0.67	0.76
U12	0.92	0.93	0.94	0.90	0.95

ilar to the original images. Interestingly, when we analyze the two resulting confusion matrices from the second evaluation method (one using GANs and the other using CGANs with augmented real data in a 3:7 ratio), we notice minor differences. Despite using GANs to augment the dataset, the performance improvement of the CNN is just slightly better, about 0-1%, compared to using CGANs. This is intriguing given that GANs require about 8 hours of training per label, whereas CGANs can train across all labels simultaneously in the same time frame. This small perTable 4: Results from the pre-experiments investigating the difference in synthetic images generated by the GANs vs. the CGAN based on a subset of three users (U1-U3). Shows the Fréchet inception distance for each user and both kinds of generated data.

User ID	GANS	CGANS
U1	11	23
U2	10	18
U3	12	29

formance gap prompts us to consider the efficiency of these two training approaches.

For the experimentation conducted on the complete dataset enriched with CGAN-generated samples, our approach began with the integration of 10% augmented data alongside the authentic images. The outcomes demonstrated an initial marginal enhancement of 1-2% across at least 8 out of the 12 users. To provide further insight, we present the sensitivities pertaining to various blends of real and augmented data in Table 2 and 3. However, as the augmentation escalated to encompass 50% augmented data and 50% real data, a decline in results became evident, indicative of overfitting. This phenomenon was illustrated by user U1, where the sensitivity dropped from 96% with only real data to 94% upon introducing 50% augmented data. This pattern was echoed across numerous labels, reflecting a decrease in accuracy by 3-4%.

Interestingly, a turning point was observed when we employed 30% augmented data and 70% real data. This configuration yielded promising outcomes, showcasing a consistent rise in sensitivity across all 12 users. Optimal results materialized when we strategically utilized CGAN-generated synthetic data to bridge gaps in labels that required additional instances to achieve a balanced dataset of 1,000 images per user. Notably, some users, like U4, U5, U6, and U12, already possessed over 1,000 images, rendering augmentation unnecessary. However, users such as U1, U2, and U3, who required a modest influx of CGAN-generated images to attain the 1,000-image threshold, experienced modest performance improvements ranging from 0-3%.

Employing this methodology yielded a general augmentation in sensitivity for all users. Particularly remarkable were the advancements in sensitivity achieved for labels U9, U10, and U11, which exhibited increases of 6-10% using this approach, as meticulously illustrated in Table 2 and 3. This underscores the efficacy of judiciously introducing CGAN-generated data to enrich datasets, resulting in substantial improvements across diverse users and labels.

# 4 CONCLUSIONS

This work has presented a data augmentation approach to increase the size of training data for better accuracy in investigating biometric properties in blood flow sounds using GANs and CNN. Previously, the CNN model had given less sensitivity per class, where some users have comparatively less data. So, we tried adding data generated by GANs and CGANs to evaluate if this leads to an improvement. When comparing results from GANs and CGANs in a pretest on data from three users, it turns out that GAN generates samples that are more similar (represented by a lower FID) to the original samples than those generated by CGANs. On the other hand, the training of a GAN for one label from the presented dataset takes 8 hours, whereas a CGAN is trained for all 12 labels at the same time. So, the GAN's output is slightly more reliable but time consuming, whereas the CGAN has the advantage of producing multilabelled output and therefore taking much less training time.

Synthetically increasing the size of data using these presented methods can be beneficial in a limited data domain. This study was mainly focused on its application on CWT images of audio data, but the concept can be expanded to other data domains. For future work, it would be interesting to also differentiate between correctly and incorrectly classified generated synthetic data. For GAN and CGANs to perform better, more measurements from the users should be included in the analysis.

## ACKNOWLEDGEMENTS

Research funding: The authors acknowledge the financial support from the State of North Rhine-Westphalia and the European Union (EU EFRE [LS-2-2-038a]).

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