Separation Method of Atrial Fibrillation Classes with High Order Statistics and Classification using Machine Learning

Luís Fillype da Silva¹, Jonathan Araújo Queiroz¹, Caroline Vanessa², Allan Kardec Barros¹, Gean Carlos Lopes¹ and Letícia Cabral¹

¹Departament of Eletrical Engineering, Federal University of Maranhão, Av. dos Portugueses, São Luís, Brazil ²Department of Nursing, Faculdade Santa Terezinha, São Luis, Brazil

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Abstract: The electrocardiogram (ECG) is an exam that presents a graphical representation of the electrical activity of the heart. Through it, it is possible to observe the rhythm of heart beats, the number of beats per minute, in addition to enabling the diagnosis of various arrhythmias. This article aims to develop a classification model based on the beats of three groups of individuals: with atrial fibrillation, intra-atrial fibrillation and normal sinus rhythm. The methodology of extraction of characteristics based and adapted to classify Atrial Fibrillation and its subtype, Intracardiac Atrial Fibrillation. The classifications were carried out in three-dimensional space in two stages: with the application of Principal Component Analysis (PCA) and without application of it, through Artificial Neural Networks (ANN), Support Vector Machines (SVM) and K-nearest Neighbors (KNN), obtaining accuracy of 93% to 99%.

1 INTRODUCTION

Atrial fibrillation (AF) as being a supraventricular arrhythmia characterized by disorganized atrial electrical activity, secondary to multiple foci of atrial depolarization (Neto et al., 2018).

Despite recent advances in the treatment of AF, patients with this heart disease still have high mortality. This is because there are other ways that AF. It has been widely used due to the nature of its observations, as shown: the complex electrical pattern observed during AF can be explained with several waves that propagate along several routes along the atria; the available data also support a focal mechanism, according to which conductors, located mainly in the pulmonary veins, trigger and support the spread of electrical activity in the atria (Richter et al., 2010). Thus, ECG is essential to predict, detect and diagnose various heart problems, aiding in its diagnosis (Queiroz et al., 2017).

Works such as that of Kachuee et. al. (2018) proposes a method based on deep convolutional neural networks for the classification of heartbeat, capable of accurately classifying five different arrhythmias. Hullah et. al. (2020) performs a

classification of 8 types of arrhythmia also using convolutional neural networks. In Queiroz et al. (2017) studied the variability of heartbeat and provided an automatic diagnosis method for heart disease. Alhusseini et al. (2020) developed a convolutional neural network to train 100,000 AF image grids. There are still methods in the literature that classify ECG signals, as proposed in Ma et al. (2020), using the RR interval for this classification of Atrial Fibrillation.

This paper studies and proposes a method of extracting the heartbeat of all ECGs from the bases used, grouping 3 groups: individuals with signs of Atrial Fibrillation, Intracardiac Atrial Fibrillation and healthy, using high-order Statistics, and subsequently performing the classification in three Machine Learning algorithms.

2 THEORY

2.1 ECG

The ECG is essential two main types of information. First, in medicine, the cardiologist can measure the

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time intervals of the ECG to determine how long the electrical wave takes to pass through the heart's electrical conduction system. This information find out to find out if electrical activity is regular or irregular, fast or slow. Second, by measuring the strength of electrical activity, the cardiologist is able to find out if parts of the heart are too large or overloaded (Ebrahimi et al., 2020).



Figure 1: ECG.

2.2 Machine Learning

Within the innovations of data science, Machine Learnine is a class of techniques and research area that allows computers to learn as humans and to extract or classify patterns. Machines may also be able to analyze more data sets and extract data resources that humans may not be able to do. This technique allows the creation of algorithms that can learn and make predictions. In contrast to rule-based algorithms, AM takes advantage of greater exposure to large and new data sets and has the ability to improve and learn from experience, such as Neural Networks, K-nearest Neighbors (Choy et al. 2016).

2.2.1 Artificial Neural Network

Artificial Neural Networks (ANN), better known as neural networks, as complex structures interconnected by simple processing elements (neurons), which have the ability to perform operations, such as calculations in parallel, for data processing and knowledge representation (Haykin, 2001).

The author also stresses the properties and capabilities that make ANN potentially useful are: non-linearity: an artificial neuron can use linear or non-linear functions; Input-Output mapping: based on examples of input and output, the ANN is able to adapt to minimize the mapping error. Among the known structures of these models, we have the MLP (Multilayer Perceptron), which, in general, has an input layer, one or more hidden layers and an output layer. See Figure 2 for the MLP model.



Figure 2: MLP model.

In this paper, MLP was used with hyperparameter of 3 neurons in the input layer, 2 layers with 100 neurons, and 3 neurons in the output layer.

2.2.2 K-Nearest Neighbors (KNN)

KNN is one of the prospective statistical classification algorithms used to classify objects based on training examples closest to the plane. According to the authors, it is a slow algorithm, due to the model or real learning not being performed during the training phase. In this case, this set is used only to fill a sample of the space with instances whose class is known. At this stage, the vector and class labels of the user-defined constant training samples, a query or test point (unlabeled vector), and the data are classified by assigning a label, which is the most recurrent among the K samples training courses closer to that consulted point (Noi and Kappas, 2018).

In this paper, KNN with K settings equal to 10 was used for the classification of heart disease.

2.2.3 Support Vector Machine (SVM)

SVM as a powerful method to build a classifier. This method aims to create a decision boundary between two classes that makes it possible to predict the labels of one or more feature vectors. For the authors, this decision frontier, known as a hyperplane, is oriented so that it is as far as possible from the closest data points for each of the classes present. Such closer points are called support vectors, giving rise to the method name (Huang et al., 2017).

In this way, the ideal hyperplane can then be defined as that which separates the data and maximizes the margin, respecting the following equations (Huang et al., 2017).

$$wx^T + b = 0 \tag{1}$$

$$wx^T + b \ge 1 \tag{2}$$

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$$\mathbf{w}\mathbf{x}^T + \mathbf{b} \le -1 \tag{3}$$

In the above equations, w represents the values of the weights, x the input vector and the bias value. Being the Equation (1) representing the optimal hyperplane, the Equations (2) e(3) parameterizing the data that represents the classes. The explanatory Figure 3 follows.



Figure 3: SVM model.

2.2.4 Principal Component Analysis (PCA)

PCA as a statistical technique that aims at condensing information from a large set of variables correlated into some variables ("main components"), while not wasting the variability present in the data set. For the authors, the main components are derived as a linear combination of the variables in the data set, with weights chosen so that these components necessarily become uncorrelated. Each component contains new information about the data set and is ordered so that the first components account for most of the variability (Ramon et al., 2006).

Demonstrating the importance of this technique, including ECG signs, PCA is used to deal with several problems in ECG analysis, such as data compression, beat detection and classification, noise reduction, separation signal and resource extraction (Ramon et al., 2006).

In this paper, PCA is not used to reduce dimensionality, but to not correlate the data, as described in (Haykin, 2009).

2.2.5 High-order Statistics

In the early 1990s, in particular, there was an increase in interest in High Order Statistics and its applications. The application of cumulants in several fields of knowledge was verified, such as sonar, biomedicine, data processing, image reconstruction, etc (Borelli, 2018).

These statistics provide more information than is available simply provided through the mean and variance of a process. Thus, it can be said that they allow a better way to discriminate processes. So, to better understand and start an approach beyond the variance and average of the sets, using the skewness and kurtosis of the data.

3 MATERIALS AND METHOD

In Figure 4, the methodology used in this article is illustrated. The used databases were defined, separating them into 3 groups: signs of individuals with AF, individuals with intra-cardiac AF and individuals with normal sinus rhythm. The database signs were pre-processed.



Then, the features represented by high-order statistics were selected, applying the PCA, generating new data. Data with PCA and without PCA were placed as input for classifiers, in order to investigate the difference in classifications in both approaches.

3.1 Database

The Intracardiac Atrial Fibrillation Database, MIT-BIH Atrial Fibrillation Database and The MIT-BIH Normal Sinus Rhythm Database data sets, both available in Goldberger et al. 2000, were used. The database of signs of patients with AF contains 23 records, all of which are used in this analysis. The signal database of patients with intra-cardiac AF contains 8 patients, all of which are used. From the database of individuals with normal sinus rhythm, 18 patients were used.

3.2 Pre-processing

ECG signs characteristic of the DII lead were acquired. The entire duration of the signal, sampled at

a frequency of 256 Hz, was used to extract the beats of each patient for analysis and subsequent extraction of features.

After that, each selected signal was segmented to obtain the respective beat, as proposed by Queiroz et al. (2017). Thus, the beats of each group were grouped, generating three matrices, one for each group of individuals, as described in the equations below.

$$M = [Bn, a Bn, b \dots Bn, z]$$
(4)

where n represents the number of beats, equal to 190, and a to z represents the total of all columns of all beats. Concomitant to this, the mean of its set was subtracted from the sign, dividing the result by Shannon's entropy, given by the Equation (5).

$$Z = M - \frac{\sum_{1}^{N} \frac{1}{N}M}{-\sum_{1}^{N} \operatorname{Plog}\left(\frac{1}{N}\right)}$$
(5)

where p represents the probability associated with each beat, and Z represents the new matrix associated with the concatenation of the beats.

3.3 Feature Extraction

The extraction methodology was adapted using highorder statistics, proposed by Queiroz et al. (2017). A vector was obtained for each of the associated statistics: variance, kurtosis and asymmetry, which will be the inputs of the classifiers, represented by σ_X^2 , κ_X and λ_X , respectively. The equations that describe such statistics are described in Equation (6), (7) and (8), where E(x) represents the Expected value.

$$\sigma_X^2 = E(X^2) - ((E(X))^2$$
(6)

$$\lambda_X = E[((X - E(X))\sigma^{-1}]^3$$
(7)

$$\kappa_X = E\left[\left(\left(X - E(X)\right)\sigma^{-1}\right]^4 \tag{8}$$

3.4 Evaluation Metrics

In this article, the values of accuracy, sensitivity and specificity, described by Equation (9), (10) and (11), were used to verify the performance of the classifiers.

In the equations, TP corresponds to the number of true positives, TN to true negatives, FP to record false positives and FN to classify false negatives.

$$Accuracy = \frac{TP + TN}{TP + FN + TN + FP} x \ 100 \tag{9}$$

$$Sensitivity = \frac{TP}{TP + FN} x \ 100 \tag{10}$$

$$Specificity = \frac{TN}{TN + FP} \times 100$$
(11)

3.5 Cross-validation

Cross validation is a technique to assess the generalizability of a model, based on a set of data. In this article, the data is divided using the holdout method, which consists of dividing the data into 70 and 30 at random. 70% of the patients were used for training, 30% for testing and k-fold equal to 7.

3.6 Dataset Builded

The construction of the data set was carried out as follows. A column was created for each statistic, representing the variance, skewness and kurtosis of each beat. A label was also created, column 4 of the data set, which represents the class belonging to the respective beat. This class has a value of 1 for a healthy, 2 for intracardiac AF and 3 for AF. See Figure 6 below.

Variance	Skewness	Kurtosis	Class
1.5743e-14	-0.6562	6.6702	1
			IONS
5.4564e-05	-1.0606	4.0094	2
0.0023	-1.0679	12.1545	3

Figure 5: Data examples.

4 RESULTS

This paper analyzed the beats extracted from the ECG for patients with normal sinus rhythm, AF and signs from individuals with intra-cardiac AF, in order to classify them.

For the classification stage, matrices were generated, where each column is represented by variance, skewness and kurtosis, respectively. Such matrices were the inputs of the KNN, SVM and ANN classifiers to verify which classification algorithm has greater accuracy, sensitivity and specificity. The results were compared with PCA in the data sets and without the application of the same. See below in Figure 6, Figure 7 and Figure 8.





Figure 8: Classifiers Specificity.

5 DISCUSSION

5.1 Data without PCA

In his work, Ma et al. (2020) used the RR interval for the classification, obtaining an accuracy of 98.3%. In another study, the same authors also used the RR interval, classifying with CNN-LSTM, obtaining an accuracy of 97.21%. Alhusseini et al. (2020) developed a CNN applied to images of 35 patients, who made decisions similar to that of specialists, with 95% accuracy. Khriji et al. (2020) used ANN to classify three differents types of heart diseases too, obtaining 93.1% of accuracy. In this work, the approach of extracting features of the beats was used, with high order statistics, obtaining an accuracy of 98.95 % for ANN.

In Figure 9, 10, 11, the analysis without PCA shows that the AF data are quite grouped, as they are the same heart disease, but with different analysis approaches.



Figure 9: Beats expressed by Variance and Skewness.



Figure 10: Beats expressed by Variance and Kurtosis.



Figure 11: Beats expressed by Skewness and Kurtosis.



Figure 12: Beats expressed by Variance, Skewness and Kurtosis.

Separations that use variance as features present a good representation and achieve high accuracy in relation to other combinations. This is because kurtosis can be an appropriate approach to measure sparse signs, such as the ECG, as discussed in Queiroz et. al. (2017). It is also inferred from Figure 6 that exemplifies the construction of the dataset, that the data sets have variance and kurtosis very different from each other, justifying this result.

5.2 Data with PCA

To improve the representation of these features, the PCA was then used to rotate these data, resulting in Figure 14.

As seen in Figures 14, 15, 16, and 17, the results of the classifications with the use of the PCA were better and confirmed by the metrics of evaluation of the algorithms themselves, described in Equations 9, 10, and 11.



Figure 13: Beats expressed by Variance and Kurtosis with PCA.



Figure 14: Beats expressed by Variance and Skewness with PCA.



Figure 15: Beats expressed by Skewness and Kurtosis with PCA.



Figure 16: Beats expressed by Variance, Skewness and Kurtosis with PCA.

SVM performed better due to its easy parameter definition. For ANN, on the other hand, it is necessary to estimate and define these values very well empirically to ensure convergence and generalization capacity. That is, to achieve the best result, it is necessary to test several different architectures, increasing or decreasing the number of hidden layers, making variations in the learning rates, momentum and number of training periods.

KNN, on the other hand, because it has a slow training and it is also necessary to estimate the number of K, this algorithm had a performance below the others used.

6 CONCLUSIONS

In this paper, the effectiveness of using high-order statistics to extract characteristics and classify heart disease, such as atrial fibrillation, was reinforced. In addition, the use of data modification was shown, showing a difference in the performance of the original data and the rotated data in ECG signs. It is also concluded that although they are the same pathology, computationally FA and intracardiac FA have different features. It can also be concluded that the use of the entire beat instead of the RR interval can be a good methodology to solve this problem.

In future works, different cardiovascular diseases can be studied in the methodology and techniques can be used to improve the pre-processing, as well as apply other classifiers to evaluate the metrics, and to test hyperparameters of the classification algorithms.

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