Estimation of Physical Activity Level and Ambient Condition Thresholds for Respiratory Health using Smartphone Sensors

Chinazunwa Uwaoma¹, Gunjan Mansingh², William Pepper¹, Wenshi Lu¹ and Siyu Xiang¹

¹Center for Information Systems & Technology, Claremont Graduate University, 130 E 9th Street, Claremont, CA, U.S.A. ²Department of Computing, The University of the West Indies, Mona, Kingston 7, Jamaica

Keywords: Physical Activity, Smartphone, Respiratory Health, Signal Magnitude Area, Ambient Conditions.

Abstract: While physical activity has been described as a primary prevention against chronic diseases, strenuous physical exertion under adverse ambient conditions has also been reported as a major contributor to exacerbation of chronic respiratory conditions. Maintaining a balance by monitoring the type and the level of physical activities of affected individuals, could help in reducing the cost and burden of managing respiratory ailments. This paper explores the potentiality of motion sensors in Smartphones to estimate physical activity thresholds that could trigger symptoms of exercise-induced respiratory conditions (EiRCs). The focus is on the extraction of measurements from the embedded motion sensors to determine the activity level and the type of activity that is tolerable to individual's respiratory health. The calculations are based on the correlation between Signal Magnitude Area (SMA) and Energy Expenditure (EE). We also consider the effect of changes in the ambient conditions – temperature and humidity, as contributing factors to respiratory distress during physical exercise. Real-time data collected from healthy individuals were used to demonstrate the potentiality of a mobile phone as a tool to regulate the level of physical activities of individuals with EiRCs. We describe a practical situation where the experimental outcomes can be applied to promote good respiratory health.

1 INTRODUCTION

The importance of physical activity in promoting good health cannot be overemphasized. Rehabilitation therapy for most chronic diseases in recent times, focuses on physical activity training protocols with proven efficacy. Nevertheless, high intensity exercise performed in unfavourable environments is also known to be a common trigger of respiratory conditions such as exercise-induced asthma (EIA), exercise-induced bronchoconstriction or bronchospasm (EIB), exercise-induced rhinitis (EIR), and vocal cord dysfunction (VCD) as reported in these studies (Nielsen et al., 2013; Sinha and David, 2003). There is a limited capacity to which the respiratory system can adapt to strenuous physical training. The phenomena that affect maximum pulmonary functioning include bronchoconstriction which occurs in the intrathoracic airways and the obstruction of the upper airways (extrathoracic) during intense exercise (Bussotti et al., 2014). And despite the many benefits of regular physical exercise, it is paradoxical to note that those considered to be "highly fit individuals" are more

susceptible to respiratory limitation or distress. This technically implies that chronic exercise training results in "faulty adaptation of the lung components" which negatively affects the respiratory system (Bussotti et al., 2014, 48). Where such situation persists, the increased burden and cost of managing these conditions impact the limited health facilities, coupled with shortages of health professionals particularly in remote areas (Braman, 2006; Seto et al., 2009; Surana et al., 2008). Hence, the need to maintain a right balance by applying preventive strategies through consistent monitoring of the level of exercise and the prevailing ambient conditions that could predispose such ailments. Remarkably, recent study has proposed new architecture and protocol to enhance continuous eHealth monitoring of chronic illnesses (Lloret et al., 2017).

Though several research efforts have concentrated on the use of accelerometer sensors for activity recognition and EE measurements, not so much attention has been given to the type and the level of physical activity appropriate for specific health conditions. This paper focuses on leveraging measurements from motion sensors in smartphones to

Uwaoma, C., Mansingh, G., Pepper, W., Lu, W. and Xiang, S.

DOI: 10.5220/0008170001130120

Estimation of Physical Activity Level and Ambient Condition Thresholds for Respiratory Health using Smartphone Sensors.

In Proceedings of the 9th International Conference on Pervasive and Embedded Computing and Communication Systems (PECCS 2019), pages 113-120 ISBN: 978-989-758-385-8

Copyright © 2019 by SCITEPRESS - Science and Technology Publications, Lda. All rights reserved

determine the activity threshold suitable for persons living with EiRCs. We also discuss how variations in environmental condition can affect physical activity level and respiratory health of persons with EiRCs. The key contributions provided by this study are as follows: (i) Given that smartphones as presently configured are not able to measure oxygen consumption directly, we explore and extend the relationship between SMA and EE to determine the level of physical activity of an individual in real-time. We consider our approach more convenient and practically simple as it uses only measurements from smartphone motion sensors compared to other methods in previous studies which require using external sensors and gadgets to estimate energy expenditure with the attendant practical limitations.

(ii) We include real-time cross measurement of variations in the ambient conditions which are noted to have significant impact on the level of engagement in physical exercise by persons with EiRCs.

2 RELATED WORK

Rigorous physical activity has been observed as a major contributor to asthma exacerbation (Bussotti et al., 2014). It has been observed that asthmatics with chronic conditions manifest signs of an asthma attack during exercise (Del Giacco et al., 2015). However, there are many people without asthma who develop symptoms only during such exercises like sporting activities. Milgrom and Taussig (1999) also report that EIA has higher prevalence among children and young adults because of their inclinations to participate in vigorous activities. Though rare, fatal events such as unexpected death during sports reportedly occur more frequently among younger professional athletes than the older ones (Bussotti et al., 2014). A fact sheet from Minnesota Centre for Health Statistics (2004) corroborates these reports where the statistics has it that about 33% of identified school related asthma deaths between 1990 and 2002 occurred during sporting events or Physical Education (PE) Class.

Symptoms of VCD and rhinitis also worsen with highly intensive physical activities performed under adverse environmental conditions (Bussotti et al., 2014). It is important to emphasize here that the severity of EiRCs is related to the type and duration of the physical exertion, as well as the prevailing ambient conditions under which such exercises or activities are performed. Studies in (Bussotti et al., 2014; Del Giacco et al., 2015), observe that persons with EiRCs have airways that are very sensitive to changes in temperature, humidity, and altitude. Nonetheless, medical experts have advised that respiratory conditions arising from intense physical activities, should not be a justification to deny people an active and healthy lifestyle. Affected individuals can equally participate in sports competitions if such conditions are properly managed and controlled (Milgrom and Taussig, 1999; Bussotti et al., 2014; Del Giacco et al., 2015). The management and treatment of respiratory disorders arising during exercise can benefit from real-time and continuous monitoring; given the social, emotional and economic impact of these health conditions on active and competitive individuals as well as the general populace (Bussotti, Marco, and Marchese 2014; Randolph 1997; Newsham et al. 2002; Keles, 2002).

Studies in recent times employ accelerometerbased measurements for recognition and classification of various physical activities that can provide vital information about individual's health and functional ability (Casamassima et al., 2014; Kwapisz et al., 2011; Chung et al., 2008). Some researchers have also worked on the use of wearable sensors and heart rate monitors for activity recognition and EE estimation during non-steady states and transitions (Altini et al., 2015; Park et al., 2017). In our study, linear motion extracted from the accelerometer measurement is used to determine the patient's level of exercise or physical activity. We also included other motion sensors (gyroscope and digital compass) facilitated by a sensor fusion technique; to generate more intelligent and useful information such as postural changes which may not be provided by using only accelerometer sensor in real-time scenarios. In addition, we used the embedded hygrometer and thermometer in smartphone to record changes in ambient conditions which could contribute to respiratory distress during intense physical activity. By placing the mobile phone securely and strategically on the body trunk, the monitoring system transforms the device motion to body motion. Recordings from smartphone sensors are computed and analyzed to measure deviation from the normal baseline of measured quantities.

3 MEASUREMENTS FROM SMARTPHONE SENSORS

3.1 Monitoring Physical Activity Level

Monitoring physical activity is recommended as a therapy or rehabilitation approach for persons recovering from cardiac and other related diseases (Kwapisz et al. 2011; Chung et al., 2008). Authors in (Karunanithi et al., 2009) observed that assessment of physical activity of the patient is often by selfreporting, diary, and a 6-minute walk test (6MWT) mostly performed at the hospital exercise clinic or laboratories, using the traditional measure of Metabolic Equivalent Task (MET). Karunanithi et al. (2009) however, proposed an alternative approach to measure physical activity for a home-based care of convalescing patients, where they used MET estimates derived from accelerometer monitors for assessing patients' 6MWT.

The advantages of using an accelerometer sensor for objective measurement and estimation of energy cost by movement intensity include its small size, portability, and low power utilization. In (Karunanithi et al., 2009), the authors demonstrate that MET can be derived from accelerometer data which has a high linear correlation ($r^2 = 0.88$) with energy expenditure derived from simultaneous measurement of oxygen consumption (VO₂) via conventional gas analyzer. The accelerometer measurement is defined by the signal magnitude area (SMA) in equation (1) while the oxygen consumption is measured by the breath gas analysis. The relationship between the two quantities is shown in equation (2) (Karunanithi et al., 2009).

$$SMA = \int (AccX_{(t)} + AccY_{(t)} + AccZ_{(t)})$$
(1)
$$VO_2 = 1.1 * SMA + 5.7$$
(2)

MET values are estimated from the regression model by averaging the acceleration measurement and oxygen consumption over a period of time. The intensity of physical activities ranges from sedentary (≤ 1.5 METs) to vigorous (> 6 METs). 1 MET is equivalent to oxygen uptake while sitting "quietly" (Chuang et al., 2013; Compendium of Physical Activities, 2018).

In our study, the basic metric used in modelling the physical activity level is the movement intensity which measures the instantaneous movement acceleration obtained from signals of the smartphone's built-in accelerometer. However, since the measurement is to be obtained over a given interval rather than momentary, we considered SMA which provides an approximate measurement of energy cost. SMA has been extensively used in previous studies for two purposes - tracking or predicting energy expenditure and discriminating between active and resting states (Chung et al., 2008; Karunanithi et al., 2009). We adopted the SMA metric for the categorization of the physical activity levels because studies have shown that it has a high



Figure 1: Linear regression and correlation of extrapolated EE values from SMA measurements in the study.

linear correlation with metabolic rate (MET value), which is widely accepted as a standard measure for movement intensity and energy expenditure (Chuang et al., 2013). Table 1 shows empirically estimated SMA values based on this relationship as documented in Compendium of Physical Activities (2018). The correlation between EE and SMA values obtained from our study is shown in Figure 1. This is a replication of the study outcome in (Karunanithi et al., 2009).

Monitoring the level of physical activity of persons with EiRCs becomes necessary due to the fundamental role played by vigorous exercise in the inflammation of the lung airways (Del Giacco et al., 2015), which largely contributes to the exacerbation of these conditions. Consistent monitoring of the physical activity level of the affected persons particularly during adverse weather conditions, will help them maintain their active lifestyle and to also participate in top sporting competitions. Interestingly, moderate exercise is being recommended "as a potential therapeutic tool" for persons with EiRCs (Del Giacco et al., 2015).

Table 1: Empirically Estimated SMA Values.

SMA Range	Designated Activity Level	Examples of Activity Type
0.0 - 1.50	Sedentary	Sitting, Standing,
		Lying
1.51 - 9.0	Low	Walking, Yoga,
		Shopping, etc.
9.1-18.0	Moderate	Jogging, Hiking,
		Climbing Stair Case,
		Callisthenics, etc.
Above	Vigorous	Bicycling, Running,
18.0		Treadmill, etc.

3.2 Capturing Ambient Data

Typical circumstances that can accentuate respiratory distress during vigorous exercise are the type and level of physical activity as well as the prevailing environmental conditions. It has been reported that changes in ambient temperature and relative humidity affect the health of persons with EiRCs. Ideal ambient temperature and relative humidity for respiratory health is rated between: 69°F and 79°F – temperature; and 35% and 50% - relative humidity (Venta, n.d; BREATHE- the lung association, n.d).

Breathing in cold and dry air during heavy exercise poses a risk for the development of symptoms of EiRCs (Bussotti et al., 2014; Del Giacco et al., 2015). Embedded ambient sensors in modern mobile phones now provide direct measurement of changes in ambient temperature and humidity. Such information can be used to determine conducive weather for engaging in vigorous and prolonged physical training. In our study, the real-time capturing of ambient condition – temperature and relative humidity on a smartphone is displayed on the chart in Figure 2.



Figure 2: Measurements of ambient temperature and relative humidity captured by the monitoring device.



Figure 3: Real-time detection and classification of physical activity levels by the monitoring device.

4 EXPERIMENTAL OUTCOMES

In this section, we describe the implementation of the physical activity monitoring on a smartphone. Two quantities of interest in the activity recognition are estimated using the motion sensors. These quantities are *posture change* obtained from the orientation measurement and *activity level* provided by the linear motion parameter. The architecture and the analytical models for these two quantities are described in our previous work (Uwaoma and Mansingh, 2014; Uwaoma and Mansingh, 2018b). The linear movement is represented by the readings of the three accelerometer axes as follows:

- z-axis: captures forward movement;
- y-axis: captures upward/downward movement and
- x-axis: captures horizontal movement.

SMA (ms ⁻²)	EE (VO ₂)	Activity Level
0.986008	6.784609	Sedentary
1.94435	7.838785	Sedentary
0.879925	6.667917	Sedentary
15.5243	22.77673	Moderate
40.58631	50.34494	Vigorous
26.91364	35.305	Vigorous
21.22344	29.04579	Vigorous
2.663409	8.62975	Low
0.935883	6.729471	Sedentary
2.273131	8.200444	Low
3.30391	9.3343	Low
2.463069	8.409376	Low
2.772076	8.749284	Low
1.191858	7.011044	Sedentary
0.69416	6.463576	Sedentary
0.795958	6.575553	Sedentary
2.134268	8.047695	Low
2.250499	8.175549	Low
1.116092	6.927701	Sedentary
2.974935	8.972429	Low
2.019332	7.921265	Low
0.973806	6.771186	Sedentary
1.028279	6.831107	Sedentary
0.338428	6.072271	Sedentary
0.39571	6.135281	Sedentary
0.464635	6.211099	Sedentary
1.649994	7.514993	Low
2.114025	8.025427	Low

Table 2: Samples of recorded SMA values extrapolated to EE equivalent with designated Activity Levels.

In the experimental test that was performed on the Android platform, we used equation (1) for calculating the SMA values based on the periodical readings on each of the accelerometer's axes. The sampling period was 5000ms which produced 25 samples based on the DELAY_NORMAL accelerometer sampling rate for android devices. To eliminate the low frequency noise and drifts associated with accelerometer sensor due to its gravity component, a high-pass filter was applied to extract the linear acceleration which was the quantity used to compute the SMA values. Table 2 shows samples of SMA values recorded in real time.

For posture change, the orientation or attitude data is measured in degrees (between 0° and 180°) which is derived from the fused orientation data of the three sensors- gyroscope, accelerometer and magnetometer. Evaluating the posture of the trunk after the user has undergone a burst of energetic or vigorous exercise helps to ascertain if there are remarkable degree of posture variations in terms of the user bending forward or tilting sideways in order to get sufficient air in the event of airway obstruction. The activity level recognition algorithms have been implemented in real life as shown in Figures 3 and 4. The y-axis in Figure 3 displays the acceleration measured in meter per second squared (ms⁻²), while the x-axis displays time in milliseconds. The line plot in magenta represents the SMA for a given period.

Below is a pseudocode implemented in Android program code used to generate the information displayed in Figure 3:

Set up a counter for each activity level detected Initialize each of the counters to zero Initialize the total duration in (ms) for each activity level to zero Define the sample period (Android sampling rate for DELAY NORMAL is assumed here) Set the current activity level to an empty string Compute the SMA value for each sampling period //Compare the SMA values with the defined ranges for each activity level if (SMA value > 0.0 and <= 1.5): Increment sedentary_counter sedentary total duration = sedentary counter * sample period Convert sedentary_total_duration to (HH:MM:SS) Set current_activity_level to "Sedentary" else if (SMA value > 1.5 and <= 9.0): Increment low counter low_total_duration = low_counter *

low_total_duration = low_counter *
sample_period
Convert low_total_duration to
(HH:MM:SS)
Set current_activity_level to
"Low"

else if (SMA value > 9.0 and <= 18.00): Increment moderate_counter moderate_total_duration = moderate_counter * sample_period Convert moderate_total_duration to (HH:MM:SS) Set current_activity_level to "Moderate"

```
else if (SMA value > 18.00):
    Increment vigorous_counter
    vigorous_total_duration =
    vigorous_counter * sample_period
    Convert vigorous_total_duration to
    (HH:MM:SS)
    Set current_activity_level to
    "Vigorous"
```

```
Return current_activity_level
```

EiRCs such as EIA and EIB are associated with shortness of breath. For instance, it has been observed that person experiencing asthma distress tends to lean forward in an effort to get sufficient air into the lungs; which invariably makes the person assume an inclined position (Uwaoma and Mansingh, 2018b; WebMD, n.d.).The implementation of the algorithm for postural changes is yet to be tested in real-time; however, we modelled the outcomes graphically as shown in Figure 5. In the model we used the z- axis orientation or tilt angle from the sensor fusion to classify bodily position into four categories:

- Upright position
- Leaning
- Lying
- Inverted



Figure 4: A bubble chart displaying the intensity aggregate of each activity level at given hours of the day.



Figure 5: Graphical Modelling of Postural Change.

5 SITUATIONAL APPLICATION OF THE PRELIMINARY RESULTS

Here we illustrate a typical practical situation where the preliminary results from the experimental tests can be applied. Asthma persistence and severity are reported to be associated with weight gain in both the paediatric and adult population. (Boulet and Cormiers, 2007, American Lung Association, 2016). Given a scenario where an individual has been diagnosed with obesity and one of the recommended therapies by the physician is regular body exercise; yet, this individual is also diagnosed with a respiratory condition – EIA. Two questions that beg for answers are: Would the patient discountenance the recommended therapy so as to avoid aggravating the respiratory condition? or would the patient engage in prolong body training despite his respiratory condition so as to lose weight as fast possible? The answer to both questions is NO. How to maintain a balance between the two options is where continuous monitoring of the individual's level of physical activity comes into play.

Using the proposed framework, the monitoring device can identify the type and level of physical activity, posture changes, as well variations in the ambient conditions that are not conducive for the individual's respiratory condition, and then signal warnings for the person to take necessary actions to avert exacerbation of his or her condition. Comprehensive details on how the monitoring tool would work to provide such vital information is described in (Uwaoma and Mansingh, 2018a).

6 CONCLUSIONS

In this study, we described a framework for determining physical activity threshold for respiratory health, particularly for persons living with EiRCs. We demonstrate how smartphones can be configured to provide a user with vital information with respect to his activity level while engaging in a physical exercise as well as changes in ambient conditions that may contribute to the exacerbation of respiratory distress during physical activity. The major advances include the ability of the proposed system to concurrently capture the two measurements emphasized here - physical activity level and variations in the environmental parameters, benchmarked on standard measures in the study domain. To the best of our knowledge, we are yet to find related work that have considered this approach. However, the focus was on maintaining a balance between engaging in regular physical exercises and managing respiratory ailments that may result from such exercises. This is an on-going study and in our future work, we hope to incorporate measurements like respiratory rate which is a known useful metric for determining a person's respiratory health status.

REFERENCES

- Altini, M., Penders, J. and Amft, O., 2015. Estimating Oxygen Uptake During Non-Steady-State Activities and Transitions Using Wearable Sensors. *IEEE Journal* of Biomedical and Health Informatics, 20(2), 469-475.
- American Lung Association, 2016. The Link between Asthma and Weight, viewed 20 May 2019. https://www.lung.org/about-us/blog/2016/07/the-linkbetween-asthma-weight.html.
- Boulet, L.P. and Cormiers, A.D., 2007. The link between obesity and asthma: a Canadian perspective. *Canadian Respiratory Journal*, 14(4), 217-220.
- Braman, S. S., 2006. The Global Burden of Asthma. *Chest Journal* 130(suppl_1), 4S-12S.
- BREATHE the lung association. n.d. *Heat and Humidity*, viewed 20 May 2019. https://www.lung.ca/news/ expert-opinions/pollution/heat-and-humidity.
- Bussotti, M., Di Marco, S. and Marchese, G., 2014. Respiratory Disorders in Endurance Athletes–How Much Do They Really Have to Endure? *Open Access Journal of Sports Medicine* 5, 47-63.

- Casamassima, F., Ferrari, A., Milosevic, B., Ginis, P., Farella, E. and Rocchi, L., 2014. A Wearable System for Gait Training in Subjects with Parkinson's Disease. *Sensors*, 14(4), 6229-6246.
- Chuang, F.C., Yang, Y.T.C. and Wang, J.S., 2013. Accelerometer-based Energy Expenditure Estimation Methods and Performance Comparison. In Proceedings of the 2nd International Conference on Advances in Computer Science and Engineering (CSE 2013), Atlantis Press. 99-103.
- Chung, W.Y., Purwar, A. and Sharma, A., 2008. Frequency Domain Approach for Activity Classification Using Accelerometer. In Proceedings of the 30th Annual International Conference - Engineering in Medicine and Biology Society (EMBS 2008), IEEE. 1120-1123.
- Compendium of Physical Activities. 2011, viewed 05 January 2018. https://sites.google.com/site/ compendiumofphysicalactivities.
- Del Giacco, S.R., Firinu, D., Bjermer, L. and Carlsen, K.H., 2015. Exercise and Asthma: An Overview. *European Clinical Respiratory Journal*, 2(1), 27984.
- Karunanithi, M., Bidargaddi, N. and Sarela, A., 2009. Determination of 6-minute Walk Test Using Accelerometer-Based Ambulatory Monitoring Device for the Assessment of Patient's Progress in Cardiac Rehabilitation. In World Congress on Medical Physics and Biomedical Engineering, Springer, Berlin Heidelberg, 540-542.
- Keleş, N. 2002. Treating Allergic Rhinitis in the Athlete. *Rhinology* 40(4), 211-214.
- Kwapisz, J.R., Weiss, G.M. and Moore, S.A., 2011.
 Activity Recognition Using Cell Phone
 Accelerometers. ACM SigKDD Explorations
 Newsletter, 12(2), 74-82.
- Lloret, J., Parra, L., Taha, M. and Tomás, J., 2017. An Architecture and Protocol for Smart Continuous eHealth Monitoring Using 5G. *Computer Networks*, 129, 340-351.
- Milgrom, H. and Taussig, L.M., 1999. Keeping Children with Exercise-Induced Asthma Active. *Paediatrics* 104(3), e38- e38.
- Minnesota Center for Health Statistics. 2004, viewed 19 May 2015. http://www.health.state.mn.us/ asthma/documents/pppresent/pehebasics.ppt.
- Newsham, K.R., Klaben, B.K., Miller, V.J. and Saunders, J.E., 2002. Paradoxical Vocal-Cord Dysfunction: Management in Athletes. *Journal of Athletic Training* 37(3), 325.
- Nielsen, E. W., Hull, J.H., and Backer V. 2013. High Prevalence of Exercise-Induced Laryngeal Obstruction in Athletes. *Medicine and Science in Sports and Exercise*, 45(11), 2030-2035.
- Park, H., Dong, S.Y., Lee, M. and Youn, I., 2017. The Role of Heart-Rate Variability Parameters in Activity Recognition and Energy-Expenditure Estimation Using Wearable Sensors. *Sensors*, 17(7), 1698
- Seto, E.Y., Giani, A., Shia, V., Wang, C., Yan, P., Yang, A.Y., Jerrett, M. and Bajcsy, R., 2009. A Wireless Body Sensor Network for the Prevention and Management of Asthma. In *Proceedings of IEEE*

PECCS 2019 - 9th International Conference on Pervasive and Embedded Computing and Communication Systems

International Symposium on Industrial Embedded Systems (SIES'09), IEEE. 120-123.

- Sinha, T. and David, A.K. 2003. Recognition and Management of Exercise-Induced Bronchospasm. *American Family Physician*, 67(4), 769-774.
- Surana, S., Patra, R., Nedevschi, S. and Brewer, E., 2008. Deploying a Rural Wireless Telemedicine System: Experiences in Sustainability. *Computer* 41(6), 48-56.
- Uwaoma, C. and Mansingh, G., 2014. Using Embedded Sensors in Smartphones to Monitor and Detect Early Symptoms of Exercise-induced Asthma. *In Sensornets*. 145-150.
- Uwaoma, C. and Mansingh, G., 2018a. Certainty Modeling of a Decision Support System for Mobile Monitoring of Exercise-induced Respiratory Conditions. In Proceedings of the 51st Hawaii International Conference on System Sciences. 2958-2966.
- Uwaoma, C. and Mansingh, G., 2018b. Proposing A Decision Support System for Automated Mobile Asthma Monitoring in Remote Areas. *Information Technology for Development*, 24(2),301-314.
- Venta. n.d. What Is an Ideal Air Humidity Level for Health? viewed 20 May 2019. https://venta-usa.com/idealhumidity-level.
- WebMD. n.d. Signs of a Pending Asthma Attack, viewed 09 May 2015. http://www.webmd.com/asthma/ asthma-symptoms-7/slideshow-asthma-attack.