

# Interactive Anisotropic Tearing of Elastic Solids

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**Abstract:** Dynamic models to simulate tearing of soft elastic bodies are an essential element of various medical and surgical training simulators. These models are also finding increased use in film and gaming applications, where control of the quality and style of the final output is highly valued. There is a general lack of models specifically designed to control tearing patterns, and in this paper, we present our work towards a soft-body tearing method that provides simple parametrizations to control the tear independently from the elastic properties of the soft body simulation. Our parameters can influence how clean-cut or jagged the tear is, in addition to allowing anisotropic influence using an embedded fibre model in the elastic body. We also aim for a real-time implementation suitable for interactive environments. Our meshless solution is discussed in a context that is aware of the importance of unified physics solvers.

## 1 INTRODUCTION

Deformable body problems and fracturing simulations were developed originally to simulate solutions for the engineering and applied sciences fields. These methods soon found their way into the computer graphics field, applying their strengths to simulate various natural dynamic phenomenon like cloth, fluids and general soft bodies. Research that is specific to computer graphics models is geared towards stability and visual realism, as opposed to absolute theoretical accuracy. Speed and efficiency are also valued greatly when comparing methods against each other. These developments find their primary application in film, game and medical simulation. We present a method to simulate fast tearing in elastic bodies that gives the user control over the fracture style and direction, while aiming at a real-time implementation for interactive environments.

While soft and viscoelastic body simulation can be done efficiently for highly dynamic real-time gaming environments, fracturing or tearing those objects apart remains a challenge at those frame rates. One efficient approach is pre-fracturing model geometries and holding the pieces together using artificial cohesive “glue” values. While this can give visually appealing results for breakable rigid bodies, it is very limiting for soft bodies that can tear at arbitrary locations. This motivated us to formulate a

soft body tearing framework that can run in interactive environments and allow independent control over the fracturing style, while interacting with the physical model used to simulate the body’s elastic behaviour.

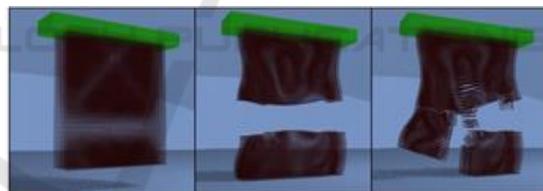


Figure 1: Stylistic control over the tearing process. Comparing the effects of  $\gamma$  on the tearing pattern, using the same elastic properties. From left to right: a) Initial state ( $t = 0$ sec); b)  $t = 0.85$  ( $t = 1$ sec); c)  $t = 0.3$  ( $t = 1$ sec).

This paper presents our research efforts towards tearable soft-body simulation with an emphasis on the following properties: First, a tearing method that provides stylistic and directional control with simple, easily implementable parameters that are independent from, but work together with the underlying material properties used for the elastic simulation. Second, have the potential for a real-time implementation without significantly compromising the accuracy of the simulation.

Finally, be based on a dynamics framework that can be embedded or extended into a unified physics solver (easy transition, extension and coupling with

other physical systems like fluid and cloth dynamics.)

With those goals in mind, we set out to achieve the following:

Extending Becker et al.'s Smoothed Particle Hydrodynamics (SPH) elastic simulation framework (2009) to support topological changes through tearing (or fracture, terms used interchangeably). Their meshless framework was chosen for its realistic simulation of elasticity at real-time rates while also being extensible to fluid and rigid simulation, as previously demonstrated by (Solenthaler et al., 2007).

Proposed the concept of a fracture disk that is inserted at any point of fracture throughout the simulation domain and, with the aid of an empirically developed transparency map, affords the end user a degree of control over the style of the tear (sharp and clean-cut vs. soft and feathered), decoupled from the elastic properties of the soft body being torn.

To control the tearing direction, we propose an anisotropic tearing model that uses a vector field, called fibres, to influence the orientation of the tear in an isotropic material. We propose the use of strain-rate to modulate this influence and to avoid a completely geometric and artificial tearing pattern. We also describe a fast and simple method of maintaining the fibre field definition during the simulation, while robustly handling situations of fracture and topological changes in the material.

## 2 BACKGROUND

Since Terzopoulos et al.'s (1988) seminal work on the dynamic simulation of deformable bodies and their fracture, this area of computer graphics research has seen a rapid increase in development, focusing on stable, visually realistic and efficient methodologies for simulating various natural physical phenomenon. Specific to fracture simulation, earlier methods heavily featured the Finite Element Method (FEM) discretization, thanks to its connected mesh definition and the ease of disconnecting them wherever fracture events occurred. FEM also provided the desirable property of convergence (as the resolution of the mesh increases, the method approaches the true continuum solution) and facilitated textured surface embedding by simply treating the boundary faces of the FEM mesh as the visual surface to render. Early examples of efficient FEM fracture include O'Brien et al.'s (1999) and its extension to ductile fracture (O'Brien et al., 2002) and Irving et al.'s (2004) very stable formulation for large and even inverted mesh deformations. FEM found further practical use in real-time gaming environments (Parker and O'Brien,

2009) and specialized medical and surgical scenarios (Meier et al., 2005). However, remeshing around topological changes while avoiding the generation of irregularly shaped and problematic elements remains a non-trivial challenge for FEM methods. This is important in tearing simulation, considering the need for fracture lines that cut through the mesh at arbitrary locations.

Recent adaptive remeshing techniques (Hahn and Wojtan, 2016), have tackled this problem, some even providing a high level of control of the fracture dynamics (Pfaff et al., 2014) with convincing visual realism. Koschier et al., (2017) proposed an approach based that decouples cut geometry from the underlying FEM mesh, avoiding the need for remeshing when tearing complex-shaped objects. FEM and XFEM methods are still, however, far from any real-time implementation, making them unviable for interactive environments.

An approach proposed in Chen et al.'s work (2014) comes closest to our goals of providing visual control over the cut features. While fast, it contrasts to our proposed method in two aspects. First, their approach is done in a post-process that modifies the FEM mesh geometrically while ours is done during runtime. Second, our approach relies on a meshless physics formulation.

Meshless methods have attracted attention for their flexibility and resampling freedom. In essence, the domain is discretized into disconnected particles (nodes) where the dynamic properties are evaluated, and each has an influence on the rest of the continuous body that decreases as we go further away from it. They do not suffer from the remeshing problems of FEM methods and have been found particularly useful for fracture simulation. Müller et al. (2004) used moving least squares (MLS) to calculate a first-order-accurate estimation of the deformation gradient and successfully showcased the versatility of meshless methods in handling elastic, plastic and viscoelastic simulation seamlessly in the same framework and at interactive rates.

Smoothed particle hydrodynamics (SPH) is a meshless method, originally developed a few decades ago to model cosmo-galactic events (Gingold and Monaghan, 1977), that later became very popular in computer graphics for real-time Lagrangian fluid simulation due to its ability to handle rapidly changing neighbourhoods with high temporal coherency and stability (Müller et al., 2003; Tan and Yang, 2009). Solenthaler et al., (2007) devised an SPH framework to model a relatively large variety of physical phenomenon including rigid, deformable and fluid objects. However, their elasticity

formulation suffered from being rotationally variant, causing incorrect handling of rotating elastic bodies that relied on an initial reference position. This was later corrected by Becker et al., (2009) in their corotated SPH formulation for elastic bodies.

Liu et al., (2011) presented a meshless method to simulate fracture in brittle solids. They used rigid dynamics for regular simulation and the Meshless Local Petric Galerkin (MLPG) method to evaluate stresses throughout the body during a fracturing event. User control over the fracture pattern was allowed through a custom weighted vector field to guide the clustering part of their algorithm. While this approach is fast and works well for brittle fracture in rigid solids, it also forces the creation of a new partition at every fracturing event, making it unsuitable for our elastic soft body tearing where partial cuts are allowed.

One of the few real-time medical simulators that provides anisotropic tearing is Allard et al.'s cataract surgery simulator (2009). In their implementation, they use a 2D FEM model along with a vector field (they called fibre field) to define the desired direction of tear propagation. In contrast to the previously discussed methods, however, their approach is purely physical, relying on a complete anisotropic elasticity simulation, which in turn directly results in anisotropic tearing simulation. While their results are convincing, their method does not allow for anisotropic fracture control in isotropic materials.

The proposed method presented in this short paper is largely based on work first introduced in (Hesham, 2011) which incorporates tearing into Becker's (2009) corotated SPH approach, and further influenced by the concepts in Allard et al.'s (2009) and Liu et al.'s (2011) research.

### 3 METHODOLOGY

We start by describing how fracture is visually encoded using fracture disks and allowed to exist in semi-arbitrary locations, followed by parametrizations that allow control over the visual detail of the fracture pattern without disturbing the underlying physical mechanics and finally, incorporating controllable anisotropic influence on the tearing direction. We apply our tearing modifications while striving for minimal impact on the computational cost of the already efficient elastic simulation.

## 3.1 Tearing

### 3.1.1 Fractured Kernel Shape Functions

In FEM or Mass-Spring System (MSS) simulations, the discretized simulation nodes have well defined connections that can be removed or split apart to introduce fracture and topological change into the model. Meshless methods like SPH, on the other hand, do not have this kind of explicit connectivity between its smoothed particles. What we can do, however, is modify the weighted kernel shape functions, such that nodes separated due to fracturing no longer continue to influence the displacement field gradient calculation, even if those nodes are still within each other's neighbourhood radius  $h$ .

For this purpose, Baleytshko et al., (2003) introduced discontinuities in the SPH kernel shape functions using a visibility criterion. Two nodes within each other's neighborhoods can no longer interact with each other if the ray passing through them intersects a crack surface. This prevented the shape functions from crossing the crack, but introduced abrupt discontinuities in  $\nabla \mathbf{u}$  on both sides of the crack, not just across it. This prompted Organ et al., (1996) to introduce transparency to the visibility check, providing a smoother outcome for the modified shape functions and better transitions near the tip of the crack front. We follow this approach and develop our own transparency criteria, motivated by empirical results and the afforded controllability of the tearing style.

Every particle  $i$  stores a visibility value  $A_{ij} \in [0, 1]$  for every particle  $j$  in its neighbourhood, where 0 means the particles can completely see each other and 1 indicates no visibility at all. This is symmetric, so  $A_{ij} = A_{ji}$ . The value is used to artificially increase the distance between  $\mathbf{x}_i^0$  and  $\mathbf{x}_j^0$  for the kernel computation in equation for both particles. So, the new distance metric used for  $r$  becomes:

$$r_{ij} = \|\mathbf{x}_i^0 - \mathbf{x}_j^0\| + A_{ij}h \quad (1)$$

A crack surface is defined as a round disk centred at position  $\mathbf{c}$  with axis vector  $\mathbf{a}$  and radius  $k$ . Whenever a fracture event is detected, a new disk is inserted. The criteria for determining the disk location and orientation is discussed in sections 3.1.2-3.2.2. Once inserted, we trigger a visibility check for all nearby particles: for a given particle  $i$ , we trace a ray to each of its neighbours  $j$  and denote the location of intersection of each ray with the fracture disk as  $\mathbf{d}_{ij}$ . The opacity  $\alpha_{ij}$  at that point on the disk gets added to the principle opacity  $A_{ij}$ . The opacity  $\alpha \in [0, 1]$  is radially defined on the disk as:

$$\alpha = \begin{cases} 1, & \|\mathbf{d}_{ij} - \mathbf{c}\| \leq \gamma k \\ 1 - \left( \frac{\|\mathbf{d}_{ij} - \mathbf{c}\| - \gamma k}{k(1 - \gamma)} \right)^e, & \text{otherwise} \end{cases} \quad (2)$$

where  $\gamma \in [0, 1]$  defines the rigidity of the fracture giving the user control over how the fracture propagates locally. Visually,  $\gamma k$  can be thought of as the radius of an inner disk that is completely opaque ( $\alpha = 1$ ) and the rest of the disk gets gradually more transparent as we move closer to the outer edge, radius  $k$ , of the disk. Figure 2 shows the gradual effect of disk transparency on the kernel shape function for particle  $i$ .

The  $\alpha_{ij}$  value is the same for both particles ( $\alpha_{ij} = \alpha_{ji}$ ). If multiple disks are inserted in the same time step (frame) of animation, the  $\alpha_{ij}$  obtained from all the disk visibility checks are treated additively and  $A_{ij}$  is updated before discarding all the disks at the end of the frame.  $A_{ij}$  can only increase, as we treat fracture damage as permanent, and once it reaches 1, the particles are dropped from each other's neighbourhood lists and are never used again in each other's  $\nabla \mathbf{u}$  calculation. Also, as a general rule, if the particles become too distant from each other  $\|\mathbf{x}_i - \mathbf{x}_j\| > 2.5h$ , we drop them from their corresponding lists, regardless of  $A_{ij}$ . Note that while the visibility check is done using the current deformed state with positions  $\mathbf{x}_i$  and  $\mathbf{x}_j$ , the neighbourhood update is done on the initial state  $\mathbf{x}_i^0$  and  $\mathbf{x}_j^0$  as that is where the elastic structure is originally defined.

High  $\gamma$  values produce very rigid and clean cuts, whereas lower values produce softness in the fracture lines and interesting patterns will arise (Figure 3 and Figure 1). Of course, values can also be defined globally or specified locally per node. We empirically found  $\gamma = 1$  to be a suitable default value.

The method presented in this section is a simple user-friendly way to alter the dynamic style of fracture, affording flexibility of design and working alongside (without being restricted by) the physical parameters used for elasticity simulation.

### 3.1.2 Fracture Criteria

Fracture or tearing is initiated at any point in the body where the maximal eigenvalue of the stress tensor exceeds the material threshold. For an isotropic material, the crack is propagated orthogonally to the corresponding eigenvector.

The stress criteria are evaluated at every particle in the simulation and we can directly begin the crack at the location of that node. However, arbitrary crack locations that are not dependent on the particle

distribution are also very easily. Part of what makes meshless methods attractive for fracture simulation is their inherent flexibility with resampling, allowing the freedom to insert particles without worrying about proper remeshing as with FEM methods.

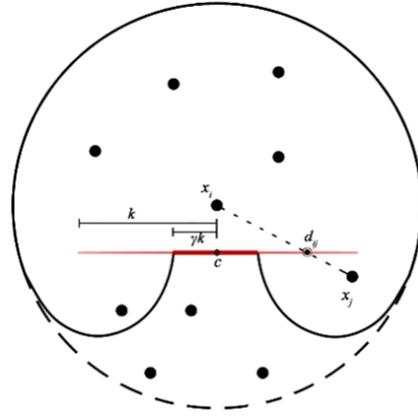


Figure 2: Effect of a visibility check through a fracture disk (red) on the kernel shape function (thick line) with influence radius  $h$  (dotted circle).

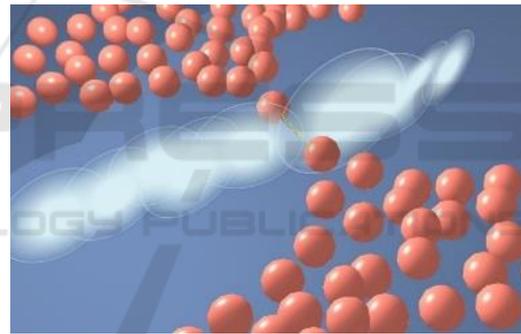


Figure 3: Effect of transparent fracture disks on the fracture style. High  $\gamma$  values produce stiff fractures akin to brittle fracture; while low  $\gamma$  produces “softer” tearing, with interesting small-scale effects like shown here, where part of the fractured object still seems to be “hanging by a thread”, as seen when tearing a fibrous body (e.g. an orange).

Our goal is still primarily an interactive application, and although resampling might increase accuracy, it could result in an unpredictable increase in the number of simulation nodes and effectively penalize simulations with a high count of fracturing events.

Our crack location method begins with a node whose principal stress (eigenvalue)  $v_i$  has exceeded the material fracture threshold. We obtain the corresponding stress eigenvector  $\sigma_{v_i}$  and the orthogonal fracture direction  $\mathbf{z}_i$ . A fracture disk is inserted with  $\mathbf{c} = \mathbf{x}_i$ ,  $a = \sigma_{v_i}$  and  $k = h + 2(v_i - \tau)$ .

We then split the neighbourhood of particle  $i$  into *Left* and *Right* neighbourhoods by the plane containing  $\mathbf{z}_i$  and whose normal is in  $\sigma_{v_i}$ . The weighted average of the maximal stresses is calculated for each side independently as *Left* and *Right*:

$$\bar{v}_{Left} = \sum_j m_j v_j W(\|\mathbf{x}_j - \mathbf{x}_i\|, h) \quad (3)$$

, for every  $j$  to the 'left' of  $\mathbf{z}_i$

$$\bar{v}_{Right} = \sum_j m_j v_j W(\|\mathbf{x}_j - \mathbf{x}_i\|, h) \quad (4)$$

, for every  $j$  to the 'right' of  $\mathbf{z}_i$

The main idea here is to find out which side is more stressed, and this bias informs us of where the fracture would have most likely occurred. Finally, we perturb the crack location from its original position  $\mathbf{x}_i$  along the stress vector  $\sigma_{v_i}$  by an amount directly proportional to the difference between *Left* and *Right*.

Since meshless methods are inherently denser than FEM methods, we find this minimal approach reasonable for finding a physically-motivated arbitrary crack location without sacrificing computational efficiency.

## 3.2 Anisotropic Tearing

In this section we describe the specifics related to anisotropic control over the tearing direction, using terminology analogous to fibres found in biological tissue (Allard et al., 2009).

### 3.2.1 Fibre Orientation Update

In our physics model, we allow a user-controlled vector field over the simulation particles to denote the desired directional influence on the tear propagation. Each vector is called a fibre, and is conceptualized as a 1-dimensional thread flowing through the body of the object. We assume that the fibres fill up the 3D domain of the simulation. That is, any particle lying within the continuum of the object has a single fibre passing through it, indicating the preferred direction of tearing at that particle. These threads give strength to the material along their main vector and resist tearing across it.

The fibrous structure of the object is discretized into a vector field over our existing set of simulation particles  $P$ . Every particle is initialised with the 3D vector  $\theta_i$  indicating fibre direction through that particle position. The directions can be defined globally, generated procedurally (for example following the curvature of the object), or setup by hand using 3D brushes or other manual techniques.

Linear, quadratic or quaternion interpolation can be used to find the intended fibre direction at arbitrary points throughout the domain.

As the simulation progresses and the object is deformed by elastic and external forces, we need to update the direction of the fibre to reflect the true fibre structure in the deformed state, because elastic forces do not produce local torque. This was not a problem in Liu et al.'s (2011) meshless brittle fracture simulation because they used rigid body dynamics and could correctly maintain the fibre direction throughout the simulation. Elastic FEM methods, like (Allard et al., 2009), can simply embed the fibre within each triangle (2D) or tetrahedron (3D) and track the orientation as the simplex deforms.

We initially experimented with an implicit definition of  $\theta_i$ , so for a certain particle  $i$ , we chose a neighbouring particle  $j$  such that  $\mathbf{x}_i^0 - \mathbf{x}_j^0$  as provided the closest approximation to the user input direction  $i$ . Once initialised, this link between  $i$  and  $j$  is constant throughout the simulation. This method was simple to implement, and gave a very stable non-jittery definition of  $\theta_i$ , but we soon realised its disadvantages. The first obvious problem was that the fibre structure became entirely dependent on the initial distribution of particles, hence we could not truly define arbitrary fibre directions. Additionally, having the direction coupled with a single particle  $j$  meant that  $\theta_i$ , was no longer aware of deformations on the opposite side of  $i$  and would not update the fibre at  $i$  accordingly. Lastly, further maintenance was required when a fracturing event separated  $i$  from  $j$ , requiring us to find a new suitable neighbour  $j$  for  $i$ . It quickly became apparent that this approach was not robust enough for our tearable simulation.

We opted instead for an explicit definition of  $\theta_i$  (Figure 4). Becker et al.'s (2009) corotated SPH formulation that we already use to evaluate elastic dynamics, provides a rotation matrix,  $\mathbf{R}_i$ , which encodes the local rotational variance from the initial undeformed shape. This gave us a very stable and efficient way to locally update the current fibre direction  $\phi_i$ :

$$\phi_i = \mathbf{R}_i \theta_i \quad (5)$$

where  $\theta_i$  (or  $-\theta_i$ , we do not differentiate between them) is now just the initial vector definition of the fibre, centred at  $\mathbf{x}_i$  and is no longer restricted to the distribution of the particles, and the current  $\phi_i$  is not affected by fracturing events.

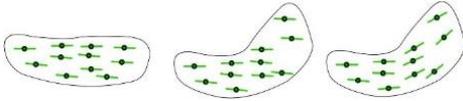


Figure 4: Fibre orientation maintenance. From left to right: undeformed particles with initial fibre direction  $\theta_i$ ; deformed particles with no update to fibre direction; deformed particles with explicit fibre update  $\phi_i = \mathbf{R}_i \theta_i$ .

### 3.2.2 Anisotropic Influence of Fibre on the Tearing Direction

In this section, we describe how fibre orientation is used to influence the fracture direction  $\mathbf{z}$  in 3.1.2, resulting in the desired anisotropic fracture.

Fibres in our simulation are there to resist tearing across the fibre's main direction. Given the plane  $\Phi_i$  whose normal is  $\phi_i$ , we want to suppress the component of the fracture vector  $\mathbf{z}_i$  in the direction of its projection onto  $\Phi_i$ . The new fracture vector is then:

$$\mathbf{z}'_i = \mathbf{z}_i - (1 - \beta_i) \text{proj}_{\Phi}(\mathbf{z}_i), \quad (6)$$

where  $\beta_i$  is a penalty term deciding the magnitude of the fibre's influence ( $0 =$  completely follow fibre direction;  $1 =$  no fibre influence at all). What distinguishes our implementation from previous penalty-based anisotropy models (Liu et al., 2011) is that in addition to allowing user-input values for  $\beta_i$ , we improve the simulation realism by also considering the physical rate of deformation (strain rate  $\dot{\epsilon}_i$ ) for varying  $\beta_i$ . The faster the rate of deformation is, the less the fibre can influence the tear's direction. The effect of our approach can be seen in Figure 5.

## 4 RESULTS

### 4.1 Implementation

We implemented our elasticity and tearing models by extending the open source SPH simulator FLUIDSv.2 (Hoetzlein and Höllerer, 2008), resulting in a system that can simulate both fluids and tearable elastic bodies. The code is written in C++ and utilizes OpenGL for graphical output.

The particles in all of our tests are on average 0.05 units apart with an influence radius  $h = 0.2$ . The number of neighbours a particle can have within its influence radius is limited to the nearest 20. This allows us to use an adjacency list to maintain neighbourhood information quite efficiently. In addition, we inserted our deforming particles into a

spatial hash as described in Viccione et al. (2008), which is a standard way to accelerate broad-phase collision detection and fluid neighbourhoods, but we also use it to quickly find the grid(s) around an inserted fracture disk, performing the disk visibility check on only those particles.

### 4.2 Performance and Results

We successfully achieve interactive rates in our tests, with our profiler indicating that our calculations take an average of 62% of the total processing time per frame, with the rest for rendering and other processes. These results, while not distinguished from similar purely elastic simulation models, show considerable speed-up when compared to similar fracturing simulations, in some cases even an order of a magnitude faster, as shown in Table 1. We do note that surfacing would incur additional costs, but our physical fracturing simulation speeds already seem promising. We compare our method with other meshless techniques in computer graphics that allow soft-body tearing. We also include the performance of Becker et al., (2009), the purely elastic framework that we extended, to show that our tearing method does not present a large computational penalty, even in situations with relatively high particle count. As the number of fractured partitions increased, our simulation got faster due to a reduced neighbourhood list. Figure 5 shows an example of an elastic soft body hanging from a static support bar (green) and getting torn by its own weight. Figure 4 shows how we enhance the realism of anisotropic tearing by considering the velocity of deformation, strain rate.

As with every physics simulator in computer graphics, stability is an important factor to consider in our tests and implementation design. We use the Verlet variant of the Leapfrog integration (Nealen et al., 2006), to advance our simulation, which was fast to solve and provided a high degree of stability. Complex cases benefited from increasing particle samples and decreasing the timestep, at an added computational cost. Generally, SPH fluid pressure forces were also useful to maintain stability for larger time steps (Becker et al., 2009; Müller et al., 2004). We also found it helpful to spread the fracture disk insertion process over several frames (4 to 10) by scaling the disk size from  $0.25k$  to  $k$ . Aside from being a reasonable reflection of reality, this had a favourable impact on our computational and visual stability.

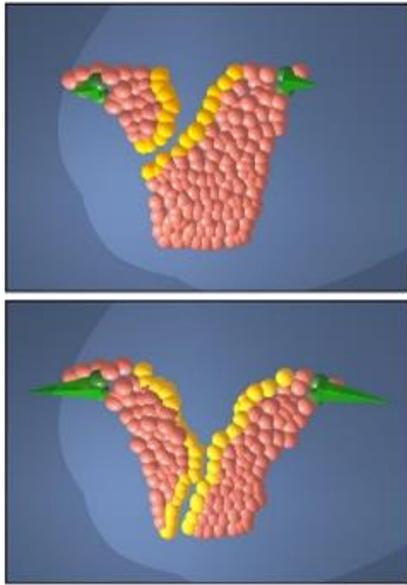


Figure 5: An originally rectangular soft body with diagonal fibres pointing north-east being torn apart by external forces (green cones). Top: peeling the object slowly allows the fibre to dictate the tearing direction. Bottom: a faster strain-rate correctly reduces the anisotropic influence of fibre, closely resembling tearing in a fibre-free object.

Table 1: Performance results for samples shown in this report.

Sample	Particles	$\gamma$ Tear Rigidity	$\Delta t$ (ms)	FPS
Figure 3.	700	0.5	5	65
Figure 5.	300	0.9	5	86
Figure 1b.	24000	0.85	5	37
Figure 1c.	24000	0.3	5	34

While evaluating our explicit fibre tracking method (Section 3.2.1), we observed that temporal coherency of the fibre orientation was not perfect (i.e. it seemed a bit jittery) for particles near the surface of newly created fractures. We believe this happens because the SPH-based rotation estimation  $\mathbf{R}$  has lesser accuracy due to a reduced number of neighbouring particles compared to the neighbours at the initial reference positions. The effect on the simulation, however, was negligible and the method is overall very sufficient for a fairly accurate and robust maintenance of fibre direction. We also noticed that it performs quite well with primarily dilation-based de-formations (stretch and compression), however it struggles to maintain the fibre orientation accurately when the object is subjected to large shear deformations. We attempted, unsuccessfully, to remedy this by extracting the local

shear information from the Jacobian of the displacement field to inform the fibre orientation. We suspect that a mixed explicit-implicit fibre update method would help greatly in this situation.

## 5 CONCLUSIONS

This short paper has presented a method for soft-body tearing that emphasizes controllability, speed and stability without significantly compromising realism and accuracy, all of which are desired aspects in game, film and medical simulation development. We provided simple parametrizations for two interesting phenomena in tearing simulation. The first, controls how clean (brittle-looking) the cuts are; and the second involved anisotropic control of the tearing direction for mechanically isotropic materials using embedded virtual fibres in the de-formable body.

We have shown how to incorporate our approach into an existing soft-body simulator by extending an elastic solids SPH framework, chosen due to the versatility of meshless methods in fracturing simulations and their suitability for extension into unified physics solvers that directly interact with other meshless simulants such as fluids.

While the observed performance of the method in this poster is encouraging, this work requires further validation against real-life scenarios, particularly building a database of parameterization for tearing of various fibrous objects (e.g. fruits and vegetables) and organic tissue. It would also benefit from comparative analysis against the established state-of-the-art in near real-time soft-body tearing. Blobby-sphere based surfacing would suffice for rudimentary examination of the results, but more sophisticated surfacing methods warrant study.

Medical soft tissue that exhibits highly non-linear and anisotropic behaviour (Zohdi, 2007) is difficult to simulate and tear accurately in real-time. This would involve extending our anisotropic component to model more sophisticated fibre fields including grids and 2D strips, in addition to accounting for anisotropy, not just in tearing, but in the mechanical behaviour itself where the material stress thresholds vary across different directions.

## ACKNOWLEDGEMENTS

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