

Methods for Quality Control of Low-resolution MALDI-ToF Spectra

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Abstract: Protein profiling of human blood serum or plasma using MALDI-ToF mass spectrometry may be used for identification of candidates for disease biomarkers. Due to many biological and technical difficulties emerging during preparation of the sample and spectra measurement quality control step is becoming important. In this study we compared different methods for finding low quality spectra based on the Pearson correlation coefficient and proposed two novel solutions. First one utilizes information about area under the measured spectrum and other incorporates modeling of signal-to-noise ratio of spectra intensity by mixture of Gaussians. Obtained results show that removing of outlying samples increases the similarity of spectra obtained within the same experimental conditions. What is more important it increases reproducibility of peak detection by decreasing the coefficient of variation of peaks intensities within a group and increasing its prevalence. This work shows that appropriate identification and removing of low quality spectra is a necessary step in analysis of mass spectrometry data and proposed tools are appropriate for quality control of MALDI-ToF data.

1 INTRODUCTION

Matrix-assisted laser desorption and ionization time of flight (MALDI-ToF) mass spectrometry (MS) can detect components at a very low concentration levels, which offers opportunities to discover diagnostic markers for a number of major diseases including cancer. Human blood serum or plasma may capture proteins and their fragments released from all organs and tissues in different conditions. Investigating of serum/plasma proteome using MALDI-ToF MS called proteome profiling can be used for identification of panels of marker candidates (Palmblad et al., 2009). Due to requirements of low cost and high speed of measurements obtained spectra are low-resolution data and do not contain the isotopic envelope of peaks.

Highly automated acquisition of a large number of data increases the risk of receiving poor quality signals. MALDI-TOF results may also be weakened by inadequate deposition of the sample on the plate, poor cleaning of the plate between runs and other technical factors. Quality control (QC) is a first important step in data analysis. Detection of the spectra with low signal-to-noise ratio (SNR) allows eliminating heavily noisy data from further analysis preventing false discoveries of candidate markers which can lack biological relevance. It is important to properly exclude

outlying spectra to guarantee the reliability of discovered patterns and reproducibility of MALDI-ToF experiments.

The easiest and fastest way of quality control is the visual inspection of measurements heat maps. Different colors are used to depict the intensity of individual spectra, which are arranged in successive rows on the graph (Figure 1). In the proteome profiling using human specimens most major peaks should be visible on all spectra, so it is possible to visually determine outliers. This method is also effective to check the quality of calibration of the mass spectrometer. Another way of QC is to use the area under the curve of the whole spectrum (total ion current, TIC). Number of ions that reach the detector at the same experimental conditions and with use of the same laser power should be similar. It is assumed that only small deviations in the values of TIC for the spectra obtained in one experiment should be observed. A useful approach to check data similarity is to calculate the Pearson correlation coefficients between the raw spectra, and then plot a correlation matrix (Hong et al., 2005) or use the diagnostic plots (Whistler et al., 2007) to find spectra which measurements are different from the others. Another group of methods involves placement of control signals in analyzed sample. Such information may be used to check only existence of control peaks or in more so-

phisticated methods like principal component analysis models. It was proved that using statistical methods on control peaks is more reliable and suitable for a large number of spectra (Coombes et al., 2003). Since most human cells, despite the variety of functions in the body, are very similar to each other in terms of its structure, it is possible to define a standard set of proteins that are present in most experimental conditions. In this way we can define a positive control for start-up of the mass spectra, which may indicate poor performance of real peak detection (Slany et al., 2009).

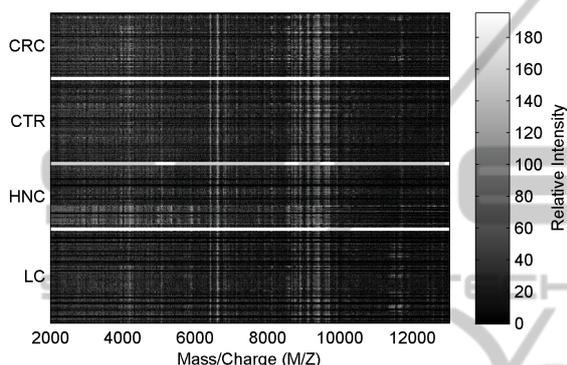


Figure 1: Heat map for 3 cancers dataset.

In this study we investigated methods for finding the low quality MALDI-ToF spectra which can be used directly on the measured signals as a first step of mass spectra analysis pipeline. We chose two procedures from the literature that are using the Pearson correlation coefficient and introduced two new algorithms: one using an outlier detection algorithm on TIC and one using a Gaussian mixture modeling (GMM) on a robust version of SNR. We analyzed the effect of using different quality control algorithms on the integrity of the spectra within a group and its influence on performance of peak detection.

2 MATERIALS AND METHODS

2.1 Data

Three different MALDI-ToF datasets obtained for proteomic profiling were used to compare quality control algorithms: 3 cancers dataset, larynx dataset and ovarian dataset. First dataset consists of 120 cancer patients from which 35 patients are with squamous cell cancer located in head and neck region (HNC), 35 patient are with colorectal cancer (CRC) and 50 patients are with non-small cell lung cancer (LC) and 45 volunteers in control group. Samples

were collected before the start of a therapy of patients and measured using 4 technical replicates of the same sample giving 659 spectra (1 damaged file). Spectra were recorded in the mass range between 2 and 13 kDa (Pietrowska et al., 2012). Second dataset consists of 54 patients with a squamous cell cancer located at larynx. Blood samples were collected before the start of therapy (sample A), 2 weeks after the start of radiotherapy (sample B) and 46 weeks after the end of radiotherapy (sample C). Not all patients had taken samples B and C. There were 4 technical replicates of each sample giving 620 spectra in total. Spectra were recorded in the mass range between 2 and 13 kDa (Widlak et al., 2011). Third dataset consists of 93 ovarian cancer patients and 77 normal blood serum samples. Spectra were recorded in the mass range between 3.5 and 20 kDa (Wu et al., 2006).

3 cancers and larynx datasets were kindly provided by the authors of the original research articles (Pietrowska et al., 2012)(Widlak et al., 2011) only for testing different QC algorithms. Ovarian cancer dataset was downloaded from <http://bioinformatics.med.yale.edu/MSDATA2>.

2.2 Spectra Pre-processing

Mass spectrum pre-processing involves removal of a measurement error, while retaining the essential biological information contained in the sample. It is an obligatory step to appropriately extract signal peaks which describe composition of analyzed material (Hilario et al., 2006). First, spectra are resampled to a common M/Z interval. Next, in baseline correction step we estimate the noise within multiple shifted window and regresses the varying baseline to the window points using a spline approximation. Spectra are aligned using peak alignment by fast Fourier transform algorithm (Wong et al., 2005) modified by introducing values of parameters to be relative to mean M/Z of analyzed segment. To detect signal peaks we used algorithm based on transforming signal into wavelet space from MassSpecWavelet package (Du et al., 2006).

2.3 Algorithms for QC

In (Hong et al., 2005) a correlation matrix (Figure 2) was developed as a QC tool in surface-enhanced laser desorption/ionization (SELDI). It is a mass spectrometry method which differs to MALDI-ToF only in ionization phase, but measured signals have similar shapes and properties. The rationale behind this approach is to assume that the protein expression profiles of samples obtained in the same experimental

Table 1: Comparison of different quality control methods using a percent of deleted spectra and the median similarity in three datasets. CRC - colorectal cancer, CTR - control group, HNC - head and neck cancer, LC - lung cancer, A,B,C - groups representing different time points, CTR - control group, OVC - ovarian cancer. None - results without quality control, Corr - method based on a correlation matrix, DP - method using the diagnostic plot, TIC - method based on a total ion current, SNR - method based on a signal-to-noise ratio of spectrum intensities.

Measure	Method	3 cancers				Larynx			Ovarian	
		CRC	CTR	HNC	LC	A	B	C	CTR	OVC
Deleted spectra [%]	Corr	3.57	3.33	7.86	16.08	0.00	1.89	3.13	2.60	1.08
	DP	3.57	3.33	7.86	16.08	0.00	0.00	2.08	2.60	1.08
	TIC	3.57	3.89	7.86	16.08	0.46	0.94	0.52	7.79	4.30
	SNR	3.57	6.11	7.86	17.09	8.33	8.96	5.21	38.96	25.81
Median similarity	none	0.653	0.765	0.576	0.564	0.779	0.781	0.803	0.613	0.647
	Corr	0.680	0.785	0.650	0.695	0.779	0.791	0.815	0.632	0.652
	DP	0.680	0.785	0.650	0.695	0.779	0.781	0.811	0.632	0.652
	TIC	0.680	0.788	0.650	0.695	0.778	0.781	0.804	0.662	0.640
	SNR	0.680	0.801	0.650	0.697	0.777	0.780	0.804	0.757	0.695

conditions should be comparable and thus that the correlation among spectra intensities should be high. Authors of algorithm suggest that the inter-spectral correlation coefficient values of R from 0.95 to 0.97 are attainable and representative figure-of-merit for quality data in analysis of SELDI sample replicates. Due to the complexity of protein signals from human specimens and individual variability of the patients, we set new thresholds for the correlation coefficients using clustering procedure (Figure 3). Hierarchical clustering was performed on the mean correlation coefficients of the spectra intensities using a shortest Euclidean distance metric. Application of other distance metrics in most cases give similar results. Optimal number of clusters was found by maximizing a silhouette measure. Sample with mean correlation coefficient belonging to the most frequent cluster are treated as high quality spectra. The remaining spectra are suspected for poor quality and removed from further analysis.

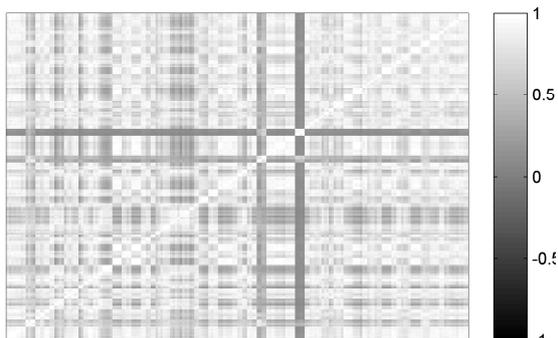


Figure 2: A correlation matrix for larynx dataset.

Another application of the idea of measuring a relationship between spectra intensities within a group is creating the diagnostic plots (Figure 4). Algo-

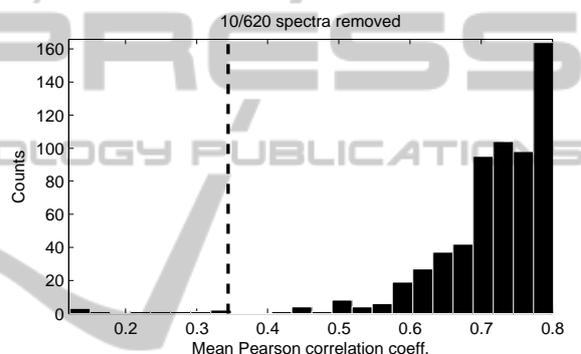


Figure 3: Histogram of the mean Pearson correlation coefficient for larynx dataset with threshold value marked by the dashed line.

gorithm of (Whistler et al., 2007) starts with generating a pairwise similarity matrix using the Pearson correlation coefficient on normalized intensity values for each spectrum. To visually depict the data, the diagnostic plot is drawn as 1 minus the mean of Pearson correlation coefficients against the range of the correlation coefficients. In our implementation due to high non-normality of distribution of the correlation coefficient we introduced robust measures of location and dispersion such as the median value and the interquartile range instead of the mean and a range. Authors of the algorithm established values of cut-off for 1- the mean of correlation coefficient by comparing the results depicted in the diagnostic plots to other evaluation methodologies, such as principal component analysis of the processed spectra or SNR, and by comparing the number of peaks in each spectrum with the average number of peaks for all spectra in the dataset. In this paper to find the cut-off value we introduced a method based on a hierarchical clustering described in a previous paragraph.

The number of measured ions for spectra in the

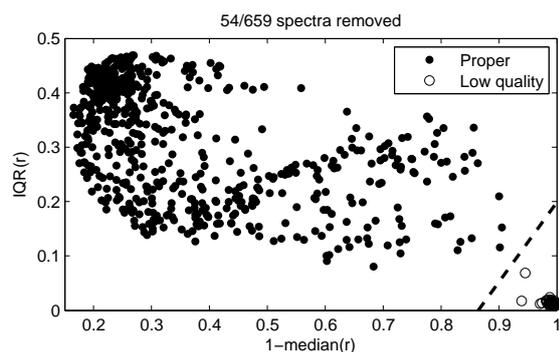


Figure 4: Diagnostic plot for 3 cancers dataset with threshold value marked by the dashed line.

same experiment should be comparable, so any meaningful deviances in area under the spectrum intensities should be treated as outlying measurements. Our studies showed that spectra with lower TIC have a negative impact on results of further analysis than the one with too high TIC due to the presence of multiple peaks resulting from noise (data not presented). To reduce skewness of distribution of TIC and extract samples with low values of TIC we initially perform logarithmic transform of TIC. Spectra with lower area under the signal are found using outlier detection method for skewed data (Hubert and Van der Veeken, 2008) on logarithm of TIC (Figure 5).

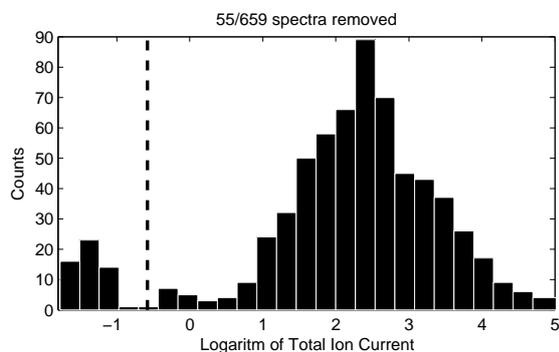


Figure 5: Histogram of TIC in logarithmic scale for 3 cancers dataset with threshold value marked by the dashed line.

SNR is a commonly used measure of the signal quality. It makes use of the mean and the standard deviation of intensities computed for each sample. These measures of location and dispersion are very sensitive to outliers. For each spectrum we have a series of tens of thousands points, only some of which are associated with significantly higher intensity values forming signal peaks. We propose to use a robust SNR measure defined as the median signal intensity to its median absolute deviation. In contrast to the classical approach of filtering data with low SNR, in our application we are looking for the samples with

too high SNR values. High value of robust SNR calculated for mass spectrum intensities indicates a large amount of only very low peaks, which may be the result of noise occurrence. To identify the cut-off value we introduced an idea of modeling the distribution of SNR using Gaussian mixture model (Figure 6). We find the optimal number of components by minimizing Bayesian information criterion. In order to distinguish Gaussian components consisting low quality spectra we use a k-means clustering procedure, which classifies estimated components into two groups by means, standard deviations and weights of Gaussian components. Then we remove samples which belong to cluster of the components located at the right hand side of the robust SNR scale (Marczyk et al., 2013).

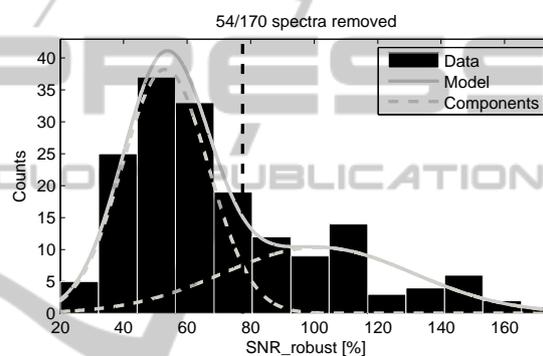


Figure 6: Histogram of robust SNR for ovarian dataset with threshold value marked by the dashed line.

3 RESULTS

Four selected quality control algorithms have been applied to study three MALDI-ToF datasets containing different number of groups and different number of spectra within a group. All procedures were applied to raw data without information of the group membership. Influence of introducing quality control as a pre-processing step on the integrity of the spectra and a performance of peak detection was obtained for data within the groups.

In Table 1 we presented percentages of deleted spectra after using different quality control tools. In some cases all algorithms remove the same low quality signals which results in the same further results (group CRC and HNC in 3 cancers dataset). For group LC all methods indicated that about 17% of data should be removed. In larynx and ovarian datasets SNR method cleaned much more spectra than other algorithms. For almost all calculations methods Corr and DP removed the same amount of data.

To quantify influence of quality control algorithms

Table 2: Comparison of different quality control methods using the median CV and a prevalence of peaks in three datasets. CRC - colorectal cancer, CTR - control group, HNC - head and neck cancer, LC - lung cancer, A,B,C - groups representing different time points, CTR - control group, OVC - ovarian cancer. None - results without quality control, Corr - method based on a correlation matrix, DP - method using the diagnostic plot, TIC - method based on a total ion current, SNR - method based on a signal-to-noise ratio of spectrum intensities.

Measure	Method	3 cancers				Larynx			Ovarian	
		CRC	CTR	HNC	LC	A	B	C	CTR	OVC
Median CV [%]	None	134.65	113.68	123.59	142.70	73.02	86.34	68.80	54.76	64.60
	Corr	130.85	109.37	109.89	120.69	72.85	80.20	68.07	52.62	64.40
	DP	130.85	109.37	109.89	120.69	73.02	86.34	68.80	52.62	64.40
	TIC	130.85	107.89	109.89	120.69	72.73	85.83	68.98	49.65	64.27
	SNR	130.85	103.54	109.89	119.76	69.38	82.66	68.45	54.03	68.16
Median prevalence [%]	none	37.86	40.56	40.71	35.68	31.48	34.91	33.59	42.86	40.86
	Corr	38.52	40.80	42.64	38.92	30.09	33.89	32.53	42.67	41.30
	DP	38.52	40.80	42.64	38.92	31.48	34.91	33.24	42.67	41.30
	TIC	38.52	41.62	42.64	38.92	30.70	34.76	34.03	40.85	40.45
	SNR	38.52	42.01	42.64	38.79	32.58	35.49	34.34	46.81	43.48

on data integrity we calculated the similarity measure (Frank et al., 2008) using all points of spectra. The intra-group similarity was defined as the median of spectra similarity calculated pairwise between the group members (Table 1). In almost all cases executing quality control step increased intra-group similarity. For 3 cancers and ovarian datasets the best results are obtained after using SNR method. For larynx dataset using Corr method gave the highest similarity.

To measure the peaks reproducibility which is a good assessment of the overall consistency of a set we first detect peaks in a mean spectrum which is constructed as the average of intensities of all spectra in a given dataset. Next, we detected peaks for an individual measurements and performed peak matching to the reference based on M/Z distance. We set a maximum considered value for the difference between peaks to $0.3\% * M/Z$. We calculated a prevalence and the coefficient of variation for the peaks intensities and summarize it within the groups calculating the median value (Table 2). In almost all cases use of quality control algorithms decreased CV and increased peaks prevalence. For CTR and LC groups of 3 cancers dataset SNR method gave the best results. In two cases Corr method gave lower CV than others. For ovarian dataset using TIC method we got the lowest CV. Introducing SNR method in this dataset lead to increased prevalence of peaks but in cost of reduced CV, which is still similar to the case when no quality control method is used.

4 DISCUSSION

Removing of low quality spectra has a big influence on increasing the amount of association between samples. Providing better similarity of data within the

same experimental group may increase reliability of protein profiling procedure. It may lead to more accurate discrimination of samples between different treatment groups and finding more significant biomarkers. Quality control also significantly increases reproducibility of experiment results by decreasing variability of estimated intensities of peaks.

It is a desirable property of QC tools that criterion for removing data is based on all samples in the dataset and disregards information on measurement group labels. Such an assumption makes this phase independent to further data analysis like searching for proteins that show different intensity levels between two groups or data classification. A violation of this condition can lead to the loss of FDR control. All methods used in this study satisfy an assumption of independence.

For two algorithms adapted from the literature we introduced a new method for separation of spectra with different quality using a hierarchical clustering. In original implementations these values were set manually by the researcher. The visual inspection of histograms of the correlation coefficients and the diagnostic plots with thresholds estimated using our method, together with presented results of analysis, proved that it is a good approach to automate process of finding cut-off values for different datasets.

Quality control process implicates reducing dimensionality of the dataset by rejecting the spectra resulting from measurement errors. In most of the applications it is proper to delete no more than 10-15% of data. In ovarian dataset SNR method removes about 30% of data which is not tolerable. This may induce a discussion if a MALDI-ToF experiment was conducted properly. However, applying of SNR method significantly increased similarity of ovarian dataset and a prevalence of peak detection, which

proves correctness of using this method. It may happen that there are too many low quality spectra in a dataset and our method allows for their appropriate control. But when the number of deleted spectra is too large in point of view of the researcher we recommend to use TIC method which also provided good results.

5 CONCLUSIONS

Applying of rigorous procedures during preparation of the sample and measurements of signal does not guarantee that all spectra from the experiment are of sufficient quality for further data analysis. In order to provide that only high quality data are used a comprehensive quality control step is required. For this purpose we recommend to use our method based on Gaussian mixture modeling of robust SNR measure. It is a fully automatic algorithm and has a potential to adapt cut-off values for removing spectra in different sets of MALDI-ToF data. Eliminating of the outlying signals with our method increases the similarity of samples measured within the same experimental conditions and reproducibility of peak detection algorithms.

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