

Statistical Analysis of Window Sizes and Sampling Rates in Human Activity Recognition

Anzah H. Niazi¹, Delaram Yazdanehpas², Jennifer L. Gay³, Frederick W. Maier¹,
Lakshmish Ramaswamy², Khaled Rasheed^{1,2} and Matthew P. Buman⁴

¹*Institute for Artificial Intelligence, The University of Georgia, Athens, Georgia, U.S.A.*

²*Department of Computer Science, The University of Georgia, Athens, Georgia, U.S.A.*

³*College of Public Health, The University of Georgia, Athens, Georgia, U.S.A.*

⁴*School of Nutrition and Health Promotion, Arizona State University, Phoenix, Arizona, U.S.A.*

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Abstract: Accelerometers are the most common device for data collection in the field of Human Activity Recognition (HAR). This data is recorded at a particular sampling rate and then usually separated into time windows before classification takes place. Though the sampling rate and window size can have a significant impact on the accuracy of the trained classifier, there has been relatively little research on their role in activity recognition. This paper presents a statistical analysis on the effect the sampling rate and window sizes on HAR data classification. The raw data used in the analysis was collected from a hip-worn Actigraphy G3X+ at 100Hz from 77 subjects performing 23 different activities. It was then re-sampled and divided into windows of varying sizes and trained using a single data classifier. A weighted least squares linear regression model was developed and two-way factorial ANOVA was used to analyze the effects of sampling rate and window size for different activity types and demographic categories. Based upon this analysis, we find that 10-second windows recorded at 50Hz perform statistically better than other combinations of window size and sampling rate.

1 INTRODUCTION

The field of Human Activity Recognition (HAR) is dependent on a variety of instruments for data collection — heart rate monitors, GPS, light sensors, etc. — of which wearable triaxial accelerometers are the most commonly utilized (Lara and Labrador, 2013), (Preece et al., 2009). Accelerometers are commercially available in many formats, from modern smartphones and consumer-grade activity-monitoring products to high-grade research-oriented devices, the consequences of which are wide degrees of quality in data collection for HAR. When preparing for data collection in a HAR study, two aspects of the accelerometer to use should be strongly considered: the placement of the device and the sampling rate at which it gathers data.

The placement of the device depends greatly on the context of the study. Many studies focusing on ambulation activities (walking, running etc.) prefer hip-worn or wrist-worn devices (Lara and Labrador, 2013), both of which have advantages and disadvantages. Wrist-worn devices have trouble distinguishing lower-body activities (for instance, walking and stair

climbing), while hip-worn devices can be problematic when recognizing upper-body activities (for instance, eating and brushing teeth). The impact of sampling rate is discussed in later sections.

Once data has been collected — typically at a fixed sampling rate — it is prepared for classification by extracting relevant features such as means and standard deviations and dividing the accelerometer readings into windows. Often, windows of fixed length are used.

Both the sampling rate and window size of data are crucial decisions in HAR which directly affect the accuracy of developed classifiers. Though a literature review revealed some relevant analyses (Section 2), there appears to be a relative dearth of work directly addressing sampling rate and window size in HAR. This study is an attempt to remedy what we perceive as a gap in the research. We have attempted to statistically identify the window size and sampling rate combination which best suits activity recognition across demographical and activity divisions.

The data used in this study was obtained from 77 demographically diverse subjects for 23 activities in studies performed at Arizona State University in

Table 1: Description of Activities Performed.

#	Activity	Duration or Distance	# of subjects
1	Treadmill at 27 m/min-1 (1mph) @ 0% grade	3 min	29
2	Treadmill at 54 m/min-1 (2mph) @ 0% grade	3 min	21
3	Treadmill at 80 m/min-1 (3mph) @ 0% grade	3 min	28
4	Treadmill at 80 m/min-1 (3mph) @ 5% grade (as tolerated)	3 min	29
5	Treadmill at 134 m/min-1 (5mph) @ 0% grade (as tolerated)	3 min	21
6	Treadmill at 170 m/min-1 (6mph) @ 0% grade (as tolerated)	3 min	34
7	Treadmill at 170 m/min-1 (6mph) @ 5% grade (as tolerated)	3 min	26
8	Seated, folding/stacking laundry	3 min	74
9	Standing/Fidgeting with hands while talking.	3 min	77
10	1 minute brushing teeth + 1 minute brushing hair	2 min	77
11	Driving a car	-	21
12	Hard surface walking w/sneakers	400m	76
13	Hard surface walking w/sneakers hand in front pocket	100m	33
14	Hard surface walking w/sneakers while carry 8 lb. object	100m	30
15	Hard surface walking w/sneakers holding cell phone	100m	24
16	Hard surface walking w/sneakers holding filled coffee cup	100m	26
17	Carpet w High heels or dress shoes	100m	70
18	Grass barefoot	134m	20
19	Uneven dirt w/sneakers	107m	23
20	Up hill 5% grade w high heels or dress shoes	58.5m x 2 times	27
21	Down hill 5% grade w high heels or dress shoes	58.5m x 2 times	26
22	Walking up stairs (5 floors)	5 floors x 2 times	77
23	Walking down stairs (5 floors)	5 floors x 2 times	77

2013 and 2014. Data was collected from a single hip-worn triaxial accelerometer, an ActiGraph GT3X+, at a sampling rate of 100Hz. By artificially downsampling the data and creating differently sized windows, we have obtained datasets at a cross section of 6 window sizes and 5 sampling rates. Multiple classifiers were tested out and random forests was selected as the standard classifier for this study. We used our standard classifier to train these datasets with 10-fold cross-validation and statistically observed the trends using repeated measures two-way ANOVA. We then further divided these datasets to observe how these effects change due to activity type or demographic features of the subject.

It should be noted that this study, by necessity, takes into account only certain aspects of HAR classification process. For example, we are utilizing data from a single hip-worn accelerometer, as opposed to other or multiple placements. Similarly, we use only time- and frequency-based features with a single classifier (Random Forests) to further standardize our tests. While feature sets and classifier selection certainly play a role in the outcomes of HAR classification research (Preece et al., 2009), to account for all of them would lead to an significant increase in complexity which could be better examined in future

research.

Section 2 details the literature available in this domain. Section 3 describes the data collection and preprocessing done to the data to obtain our data sets. Section 4 gives the results of our classification and statistical analysis of these results. Finally, Section 5 states what we conclude from this work and how these conclusions can be implemented in HAR data classification.

2 RELATED WORK

While a considerable amount of research has been done in HAR using accelerometers, there has been a lack of consensus on the methodology of collecting and preprocessing data and thus this topic has largely remained unanalyzed (Preece et al., 2009). Lara and Labrador (2013) note that sampling rates in HAR studies vary from 10Hz to 100Hz while window sizes range from less than 1 second to 30 seconds. While there are some domain-related justifications for such decisions, there is a lack of standardization which likely impacts replicability.

Lau and David (2010) attempted a study similar

to ours, in the sense that multiple data sets of differing window sizes (0.5, 1, 2 and 4 seconds) and sampling rates (5, 10, 20 and 40 Hz) were generated from raw accelerometer data (gathered from a pocketed smart phone) and the effects studied. While they claim that these lower values are sufficient for good performance, their setup consisted of a single test subject performing 5 activities. Maurer et al. (2006), using 6 subjects, state that recognition accuracy does not significantly increase at sampling rates above 15-20Hz when their biaxial accelerometer is used in conjunction with 3 other sensors (light, temperature and microphone). Bieber et al. (2009) calculate that 32Hz should be the minimum sampling rate given human reaction time. Tapia et al (2007) varied window length from 0.5 to 17 seconds and tested the data sets with C4.5 decision tree classifiers, concluding that 4.2 seconds was the optimum window size for their needs. Banos et al (2014) created data sets with window sizes ranging from 0.25 to 7 seconds at interval jumps of 0.25. They found that 1-2 seconds is the best trade-off speed and accuracy for online training. Larger windows were only needed if the feature set was small.

Statistical analysis of classifier performance appears infrequently performed. Most studies, such as the ones cited above, simply state a performance measure (often accuracies and f-measures) but do not present any statistical evaluation. Demsar (2006) comments on the lack of statistical analysis of classifier performance and prefers non-parametric tests for comparing classifiers over parametric ones. The paper also notes that replicability is a problem for most experiments machine learning domain, hence experiments should be tested on as many data sets as possible.

3 DATA COLLECTION, PREPROCESSING AND METHODOLOGY

3.1 Collecting Data

The data used in the present study was collected in Phoenix, AZ from volunteers recruited through Arizona State University. Participants were fitted with an ActiGraph GT3X+ activity monitor positioned along the anterior axillary line of the non-dominant hip. The monitor was fixed using an elastic belt. The ActiGraph GT3X+ (ActiGraph) is a lightweight monitor (4.6cm x 3.3cm x 1.5 cm, 19g) that measures triaxial acceleration ranging from -6g to +6g. Devices were

initialized to sample at a rate of 100hz. Accelerometer data was downloaded and extracted using Actilife 5.0 software (ActiGraph LLC, Pensacola, FL). The subjects performed a number of activities which can be observed in Table 1.

Data from 77 subjects (53 female and 24 male) was used to train the classifiers. The 77 subjects were taken from a larger group of 310 subjects who participated in the study. They were chosen for their relative diversity in both demographics and the activities they performed. Table 1 describes the activities performed while Table 2 provides demographic information on the subjects.

Table 2: Subject Demographics.

	Mean	Standard Deviation	Range
Age (Years)	33.2	9.7	18.2 - 63.2
Height (cm)	167.9	7.9	152.6 - 188.9
Weight (kg)	72.1	12.1	48.3 - 105.5
BMI	25.6	3.9	17.7 - 35.4

3.2 Generating Datasets

As noted earlier, the raw data was collected at a sampling rate of 100Hz. From this, 30 data sets with varying window sizes (of 1, 2, 3, 5 and 10 seconds) with sampling rates (5, 10, 20, 25, 50 and 100Hz) were created. To create data sets for sampling rates < 100Hz, we downsampled from the original data sets, e.g., 50Hz is generated by using every 2nd accelerometer record (100/50), 25Hz using every 4th record (100/25), etc. The number of records in a window then depends on the sampling rate as well as the window size. E.g., A 1-second window at 100 Hz contains 100 records (100x1), a 3-second window at 25Hz contains 75 records (3x25), and so on. As summarized in Table 3, the window size affects the number of records in the data set, a fact that will become significant during analysis.

It should also be noted that, in some situations, partial windows are formed; in these, not enough data exists to form a complete window. Such partial windows were discarded in order to provide the classifier a data set with a uniform format.

Table 3: Number of Records in the Datasets.

Window Size (s)	No. of Records
1	175284
2	88557
3	59666
5	36533
10	19186

3.3 Feature Extraction and Selection

246 features were extracted using the raw accelerometer data which were then reduced to a 32 feature data set with time- and frequency-based features. The 32 feature set was reduced through correlation-based feature selection, as well as from experts in the domain of human activity recognition. For more information on feature selection, see (Niazi et al., 2016).

- **Features in the Time Domain:** These features include the mean, standard deviation and 50th percentile of each axis (x, y and z) and their vector magnitude as well as the correlation values between the axes.
- **Features in the Frequency Domain:** These features include the dominant frequency and its magnitude for each axis (x, y and z) as well as their vector magnitude.

3.4 Methodology

Random forest classifiers perform very well with this data set (Niazi et al., 2016) and so this was chosen as our standard classifier. Each data set was divided and evaluated in 10 folds. Further divisions were carried out for certain activity groups (see Table 4) or demographic groups. The accuracy on the test fold was recorded. WEKA software packages (Hall et al., 2009) were used in conjunction with custom Java code for training and testing the data sets.

RStudio (RStudio Team, 2015) was used to evaluate results. A two-way factorial ANOVA was carried out with weighted least squares to calculate the expected average value (EV) for every combination. It was found that window size and sampling rate as well as their interaction were statistically significant. By determining the maximum expected accuracy (the maximum EV), we discovered the accuracy remained significant at the 95% confidence level. The next section details the analysis and results of our experiments.

Table 4: Division of activities in the clusters.

Non-Ambulatory Activities	
	8,9,10,11
Ambulatory Activities	
Walking	1,2,3,4,12,13,14,15, 16,17,18,19,20,21
Running	5,6,7
Upstairs	22
Downstairs	23

4 STATISTICAL ANALYSIS OF RESULTS

4.1 Weighting

From Table 3, it is clear that window size directly affects the number of records in the data set. Table 5 shows that the variance increases as window size increases, and so the weighting function should be inversely proportional to the variance. For the weighted least squares, we use $1/WindowSize$ as an approximation.¹ Although sampling rate can also be seen to have a small effect on the variance, it appears negligible. All experiments use this weighting function to normalize the distributions.

Table 5: Standard Deviations.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.0035	0.0034	0.0032	0.0029	0.0027	0.0021
	2	0.0051	0.0031	0.0048	0.0032	0.0057	0.0032
	3	0.0049	0.0071	0.0076	0.0066	0.0040	0.0054
	5	0.0045	0.0057	0.0092	0.0108	0.0107	0.0071
	10	0.0091	0.0129	0.0074	0.0082	0.0098	0.0096

How the standard deviation varies according to window size and sampling rate for the data.

Subsection 4.2 describes in detail the statistical process followed by all the experiments.

4.2 All Activities and Demographics

Our first test evaluated all the data available, i.e., for 23 activities as performed by 77 subjects. The objective was to find the maximum average expected value (EV) and use this to determine if other values can be considered statistically significant. A two-way analysis of variance (ANOVA) on a Weighted Least Squares (WLS) linear regression model shows that both window size and sampling rate have a significant effect on accuracy with 99% confidence ($p < 0.001$). The linear model is then used to obtain EVs for all window size/sampling rate combinations. These values are shown in Table 6.

Table 6: All Activities/Demographics.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.5858	0.6868	0.7893	0.8050	0.8251	0.8292
	2	0.6324	0.7355	0.8219	0.8334	0.8456	0.8435
	3	0.6544	0.7551	0.8269	0.8385	0.8488	0.8411
	5	0.6848	0.7752	0.8322	0.8379	0.8473	0.8282
	10	0.7316	0.8050	0.8474	0.8529	0.8583	0.8126

Values shown are the average expected value (EV) for accuracy on each dataset

¹The weighting scheme was chosen after a consultation with the University of Georgia Statistics Consulting Center.

The 10s/50Hz data set has the highest expected value (EV_{max}) for accuracy (in **bold underline** in Table 6) in this experiment. Next we determine if other accuracy EVs are significantly different than the maximum EV_{max} . As the alternate hypothesis is that other combinations will have lower EVs, we use a 1-sided t-test with a 95% confidence interval.

$$X_{max}^- - \bar{X}_k = t_{290,0.95} * \sqrt{MSE} * \sqrt{\frac{WS_{max}}{n_{max}} + \frac{WS_k}{n_k}} \quad (1)$$

Equation 1 is used to find the critical distance when the sample sizes are unequal but the variance is assumed equal. As each EV represents 10 folds, we have 290 degrees of freedom. The value of $t_{290,0.95}$ is found as 1.651. The MSE value is obtained from ANOVA. WS represents window size of EV_{max} while WS_k and n is the number of observations which in our case is always 10. Having found the critical distance, we can observe which EV values fall inside the margin.

In this experiment, the 10s/25Hz value (in **bold** in Table 6) is less than the critical distance away from EV_{max} . Hence, it can be concluded that it is statistically as accurate as EV_{max} with 95% confidence.

The procedure elaborated in this section is replicated for all of the following experiments.

4.3 Activity Groups

In Table 7, ambulatory activities were separated from non-ambulatory activities while in Table 8 they were classified as walking, running or stairclimbing activities. Both experiments represent a macro-classification and as such exhibit similar patterns to Table 6 — the 10s/50Hz has EV_{max} .

Tables 7-12 show the results of experiments on different activity group classifications. These groups were divided as shown in Table 4.

However, classifications at a micro-level, within these activity groups, exhibit different results. Classifying between ascending and descending stairs (Table 9) achieves EV_{max} of 97% at 2s/50Hz. However, statistically significant EVs for the experiment are spread across a wide range of window sizes and sampling rates. Interestingly data at lower sampling rates are also deemed significant for larger window sizes. Statistical values for non-ambulatory activities (Table 10) show similar patterns. For walking and running activities, the spread is smaller and concentrated towards higher sampling rates, though there is a lot of variation in window size. Running in particular prefers smaller windows. This is in agreement with the claim by Bieber, et al (2009) that the sam-

pling rate should be more than 32Hz for ambulatory activities.

4.4 Demographics

For the next round of experiments, data was separated into demographic groups to observe any significant effects. The data sets were then used to classify all 23 activities.

Division by gender, female (53 subjects) and male (24 subjects) (Tables 13 and 14 respectively) display similar results. EV_{max} is at 10s/50Hz for both experiments and there are very similar spreads in significant results. This indicates that there is an insignificant difference in HAR for genders and activity classification should be generalized for both cases.

Data was then divided into 4 age groups; 18 – 25 (24 subjects), 26 – 32 (24 subjects), 33 – 44 (21 subjects) and 49 – 63 (8 subjects). The results of these experiments are recorded in Tables 15-18, respectively. There is a visible trend of decreasing window size with increasing age. The spread of significant values gets larger as well.

Similar patterns are noted when the data is divided according to Body Mass Index (BMI) categories; Normal (40 subjects), Overweight (28 subjects) and Obese (9 subjects) (Tables 19-21). As BMI increases, the significance of the EV_{max} decreases along with the window size. Subjects with lower BMIs fare better with larger windows than those with higher BMIs. This can suggest a correlation between age and BMI - elderly people are less likely to be active than young people and are thus more likely to have high BMIs. This hypothesis is supported in Figure 1 which shows that the proportion of normal weighted people decreases with age in the dataset.

4.5 Summary of Analysis

Viewing all experiments together suggests that 10s/50Hz is the optimal combination of window size and sampling rate, especially if the subjects of the study are young, able-bodied and physically active. Most high significant EV are spread around high sampling rates and window sizes, although there is enough evidence to suggest there is not a very significant loss in accuracy if the sampling rate is decreased to 25Hz or window size is decreased to 2s.

Table 7: Ambulatory vs. Non-Ambulatory Activities.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6408	0.7295	0.8228	0.8369	0.8559	0.8590
	2	0.6812	0.7735	0.8521	0.8634	0.8754	0.8730
	3	0.7016	0.7957	0.8605	0.8688	0.8791	0.8725
	5	0.7319	0.8127	0.8656	0.8727	0.8796	0.8634
	5	0.7319	0.8127	0.8656	0.8727	0.8796	0.8634
	10	0.7792	0.8419	0.8805	0.8876	0.8913	0.8537

Table 8: Ambulatory Activity Groups.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.8345	0.8720	0.9065	0.9106	0.9165	0.9170
	2	0.8345	0.8872	0.9155	0.9177	0.9219	0.9195
	3	0.8609	0.8951	0.9181	0.9211	0.9254	0.9200
	5	0.8754	0.9045	0.9237	0.9267	0.9293	0.9180
	5	0.8754	0.9045	0.9237	0.9267	0.9293	0.9180
	10	0.9022	0.9264	0.9412	0.9411	0.9440	0.9169

Table 9: Stairs: Ascent vs. Descent.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.9555	0.9640	0.9675	0.9682	0.9690	0.9694
	2	0.9599	0.9652	0.9681	0.9686	0.9697	0.9690
	3	0.9611	0.9651	0.9670	0.9675	0.9690	0.9673
	5	0.9618	0.9655	0.9668	0.9672	0.9670	0.9647
	5	0.9618	0.9655	0.9668	0.9672	0.9670	0.9647
	10	0.9650	0.9676	0.9676	0.9690	0.9687	0.9624

Table 10: Non-Ambulatory Activities.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.7854	0.8298	0.8609	0.8647	0.8711	0.8723
	2	0.8086	0.8471	0.8726	0.8783	0.8795	0.8775
	3	0.8161	0.8476	0.8734	0.8732	0.8780	0.8746
	5	0.8246	0.8525	0.8682	0.8730	0.8726	0.8594
	5	0.8246	0.8525	0.8682	0.8730	0.8726	0.8594
	10	0.8406	0.8571	0.8713	0.8716	0.8716	0.8514

Table 11: Walking Activities.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.5556	0.6656	0.7916	0.8105	0.8329	0.8385
	2	0.5976	0.7162	0.8274	0.8407	0.8581	0.8574
	3	0.6189	0.7415	0.8344	0.8460	0.8598	0.8543
	5	0.6474	0.7594	0.8374	0.8408	0.8527	0.8353
	5	0.6474	0.7594	0.8374	0.8408	0.8527	0.8353
	10	0.6875	0.7746	0.8387	0.8491	0.8557	0.8159

Table 12: Running Activities.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.7081	0.7795	0.8522	0.8688	0.9070	0.9140
	2	0.7349	0.8191	0.8793	0.8961	0.9185	0.9210
	3	0.7418	0.8321	0.8891	0.8968	0.9176	0.9177
	5	0.7584	0.8266	0.8703	0.8863	0.8953	0.8972
	5	0.7584	0.8266	0.8703	0.8863	0.8953	0.8972
	10	0.7728	0.8333	0.8639	0.8714	0.8759	0.8553

Table 13: Gender: Female Subjects.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6037	0.7132	0.8128	0.8227	0.8405	0.8430
	2	0.6509	0.7606	0.8388	0.8490	0.8599	0.8554
	3	0.6762	0.7762	0.8433	0.8529	0.8598	0.8498
	5	0.7052	0.7937	0.8441	0.8490	0.8539	0.8351
	5	0.7052	0.7937	0.8441	0.8490	0.8539	0.8351
	10	0.7521	0.8164	0.8586	0.8595	0.8667	0.8169

Table 14: Gender: Male Subjects.

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6439	0.7248	0.8139	0.8265	0.8474	0.8508
	2	0.6857	0.7633	0.8412	0.8506	0.8653	0.8624
	3	0.7017	0.7815	0.8478	0.8569	0.8675	0.8597
	5	0.7226	0.7984	0.8484	0.8547	0.8641	0.8408
	5	0.7226	0.7984	0.8484	0.8547	0.8641	0.8408
	10	0.7759	0.8183	0.8636	0.8678	0.8736	0.8253

Table 15: Age: 18-26 Years

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6207	0.7174	0.8094	0.8236	0.8432	0.8457
	2	0.6662	0.7620	0.8362	0.8488	0.8588	0.8553
	3	0.6857	0.7824	0.8443	0.8559	0.8629	0.8551
	5	0.7196	0.8024	0.8484	0.8542	0.8623	0.8424
	5	0.7196	0.8024	0.8484	0.8542	0.8623	0.8424
	10	0.7633	0.8292	0.8627	0.8717	0.8753	0.8250

Table 16: Age: 27-33 Years

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6614	0.7513	0.8343	0.8428	0.8590	0.8618
	2	0.7043	0.7891	0.8564	0.8676	0.8746	0.8731
	3	0.7198	0.8051	0.8623	0.8678	0.8779	0.8677
	5	0.7390	0.8117	0.8573	0.8643	0.8679	0.8488
	5	0.7390	0.8117	0.8573	0.8643	0.8679	0.8488
	10	0.7784	0.8292	0.8658	0.8695	0.8720	0.8250

Table 17: Age: 34-44 Years

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6651	0.7660	0.8442	0.8547	0.8689	0.8722
	2	0.7085	0.8038	0.8654	0.8730	0.8849	0.8805
	3	0.7271	0.8193	0.8651	0.8730	0.8807	0.8696
	5	0.7482	0.8226	0.8596	0.8624	0.8721	0.8533
	5	0.7482	0.8226	0.8596	0.8624	0.8721	0.8533
	10	0.7833	0.8424	0.8733	0.8792	0.8822	0.8375

Table 18: Age: 49-63 Years

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.7593	0.8382	0.8892	0.8981	0.9065	0.9063
	2	0.7856	0.8581	0.9043	0.9084	0.9135	0.9146
	3	0.8046	0.8689	0.9040	0.9067	0.9101	0.9030
	5	0.8201	0.8730	0.9031	0.9017	0.9084	0.8855
	5	0.8201	0.8730	0.9031	0.9017	0.9084	0.8855
	10	0.8503	0.8986	0.9114	0.9114	0.9119	0.8725

Table 19: BMI: Normal

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6031	0.7074	0.8056	0.8188	0.8363	0.8393
	2	0.6531	0.7525	0.8320	0.8437	0.8531	0.8503
	3	0.6776	0.7753	0.8395	0.8493	0.8553	0.8478
	5	0.7138	0.7946	0.8446	0.8482	0.8549	0.8376
	5	0.7138	0.7946	0.8446	0.8482	0.8549	0.8376
	10	0.7617	0.8204	0.8614	0.8615	0.8678	0.8149

Table 20: BMI: Overweight

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.6419	0.7381	0.8256	0.8391	0.8564	0.8597
	2	0.6831	0.7762	0.8520	0.8609	0.8714	0.8689
	3	0.7002	0.7940	0.8523	0.8612	0.8701	0.8637
	5	0.7225	0.8064	0.8549	0.8619	0.8696	0.8494
	5	0.7225	0.8064	0.8549	0.8619	0.8696	0.8494
	10	0.7612	0.8287	0.8607	0.8674	0.8732	0.8252

Table 21: BMI: Obese

		Sampling Rate (Hz)					
		5	10	20	25	50	100
Window Size (s)	1	0.7423	0.8279	0.8803	0.8900	0.8998	0.9015
	2	0.7817	0.8532	0.9008	0.9039	0.9164	0.9115
	3	0.7968	0.8648	0.9010	0.9098	0.9167	0.9098
	5	0.8164	0.8663	0.8943	0.9001	0.9070	0.8878
	5	0.8164	0.8663	0.8943	0.9001	0.9070	0.8878
	10	0.8368	0.8774	0.8994	0.9125	0.9091	0.8648

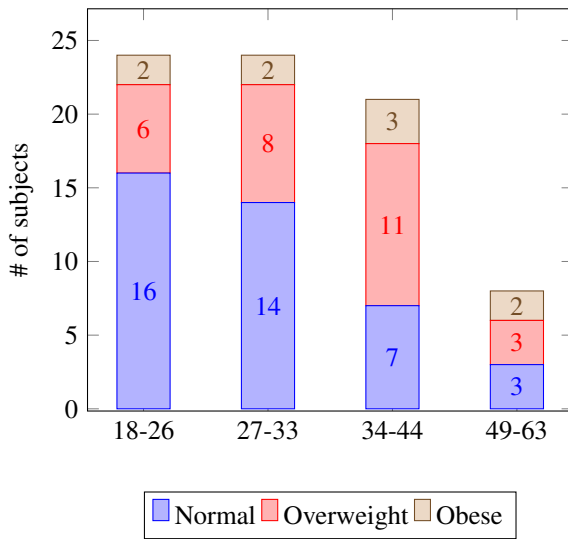


Figure 1: Distribution of BMI groups over age groups.

5 CONCLUSION

This study provides some basis for the selection of sampling rates and window sizes for human activity recognition. The analysis indicates that 10s/50Hz is statistically the best combination for data collected with a single hip-worn accelerometer. Most of the experiments carried out preferred larger windows and high sampling rates though some low intensity activities and demographics can perform better with smaller windows. Our analysis further suggests that window size can vary between 2-10 seconds and sampling rate 25-100Hz for different situations without a significant loss in performance. While our study has shown that larger windows are preferable, smaller windows can still provide significant results if power consumption is an issue. Additionally, lower values are preferable for studies involving the less dynamic activities or subjects who are more liable to be less active.

Future work in this field should be done to understand aspects of Human Activity Recognition better. This study was performed under some assumptions that can be scrutinized. The placement of the accelerometer could be shown to affect classifier performance for different activities — a combination of sensors can also be used. Other sensors, such as heart rate monitors or video image processors, provide new avenues. This study can also be replicated using different classifiers or learning methods with different feature sets. Extensive analysis on the statistical value of other machine learning and data mining methods could also help the field as a whole.

REFERENCES

- ActiGraph. Actisoft analysis software 3.2 user's manual. fort walton beach, fl: Mti health services.
- Banos, O., Galvez, J.-M., Miguel Damas, H. P., and Rojas, I. (2014). Window size impact in human activity recognition. *Sensors*, pages 6474–6499.
- Beiber, G., Voskamp, J., and Urban, B. (2009). Activity recognition for everyday life on mobile phones. *International Conference on Universal Access in Human-Computer Interaction*, pages 289–296.
- Demsar, J. (2006). Statistical comparisons of classifiers over multiple data sets. *Journal of Machine Learning Research*, 7:1–30.
- Hall, M., Frank, E., Holmes, G., Pfahringer, B., Reutemann, P., and Witten, I. H. (2009). The weka data mining software: An update. *SIGKDD Explor. Newsl.*, 11(1):10–18.
- Lara, O. D. and Labrador, M. A. (2013). A survey on human activity recognition using wearable sensors. *IEEE Communication Surveys and Tutorials*, 15:1192–1209.
- Lau, S. and David, K. (2010). Movement recognition using the accelerometer in smartphones. *IEEE Future Network and Mobile Summit 2010*, pages 1–9.
- Maurer, U., Smailagic, A., Siewiorek, D. P., and Deisher, M. (2006). Activity recognition and monitoring using multiple sensors on different body position. *International Workshop on Wearable and Implantable Body Sensor Networks*.
- Niazi, A., Yazdensemepas, D., Gay, J., Maier, F., Rasheed, K., Ramaswamy, L., and Buman, M. (2016). A hierarchical meta-classifier for human activity recognition. *IEEE International Conference on Machine Learning and Applications*.
- Preece, S. J., Goulermas, J. Y., Kenney, L. P. J., Howard, D., Meijer, K., and Crompton, R. (2009). Activity identification using body-mounted sensors: a review of classification techniques. *Physiological Measurement*, 30(4):R1.
- RStudio Team (2015). *RStudio: Integrated Development Environment for R*. RStudio, Inc., Boston, MA.
- Tapia, E., Intille, S., Haskell, W., Larson, K., Wright, J., King, A., and Friedman, R. (2007). Real-time recognition of physical activities and their intensities using wireless accelerometers and a heart rate monitor. *IEEE 11th IEEE international symposium on wearable computers*, pages 37–40.
- Yazdensemepas, D., Niazi, A. H., Gay, J. L., Maier, F. W., Ramaswamy, L., Rasheed, K., and Buman, M. P. (2016). A multi-featured approach for wearable sensor-based human activity recognition. *IEEE International Conference on Healthcare Informatics (ICHI)*, Chicago, IL.