Evaluation of the Degree of Malignancy of Lung Nodules in Computed Tomography Images

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- Keywords: Medical Diagnostic Imaging, Computer-aided Diagnosis, Computed Tomography, Machine Learning, Feature Extraction.
- Abstract: In lung cancer diagnosis, the design of robust Computer Aided Diagnosis (CAD) systems needs to include an adequate differentiation of benign from malignant nodules. This paper presents a CAD system for the classification of lung nodules in chest Computed Tomography (CT) scans as the way to diagnose lung cancer. The proposed method measures a set of 295 heterogeneous characteristics, including morphology, intensity or texture features, that were used as input of different KNN and SVM classifiers.

The system was modeled and trained using a groundtruth provided by specialists taken from a public lung image dataset, the Lung Image Database Consortium and Image Database Resource Initiative (LIDC-IDRI). This image dataset includes chest CT scans with lung nodule location together with information about the degree of malignancy, among other properties, provided by multiple expert clinicians. In particular, the computed degree of malignancy try to follow the manual labeling by the different radiologists. Promising results were obtained with a first order SVM with an exponential kernel achieving an area under the receiver operating characteristic curve of 96.2 \pm 0.5% when compared with the groundtruth provided in the public CT lung image dataset.

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1 INTRODUCTION

Nowadays, lung cancer is clearly the world's deadliest type of cancer and one of the main causes of deaths in developed countries. In Uniter States, it represents approximately the 13% of all new cases of cancer and the 27% of all cancer deaths. It presents an alarming 5-year relative survival rate of only 18% (Siegel et al., 2016). As a reference, the number of deaths regarding lung cancer is greater than the sum of the second to fourth cancers regarding deceases, that are, colon, breast and prostate cancers. Among the main causes of this situation, we can mention the difficulty in obtaining a good early diagnosis, as the diagnose is, in most of the cases, difficult due to very small size and subtlety, and poor contrast of nodules in the first stages of development. Moreover, it is a complex process demanding from the radiologists an exhaustive and tedious revision of Computed Tomography (CT) scans (Breadsmoore and Screaton, 2003; van Ginneken, 2008). This complicates possible preventive screening programs as happens, for example, with breast cancer. Given the aggressiveness of this kind of cancer, the possibility of an early diagnosis represents a crucial factor for the patient's survival rate.

From all the possibilities of medical imaging, chest CT imaging is one of the most used modalities for lung cancer diagnosis as it presents an adequate quality to identify the presence of lung nodules. Computer-aided Diagnosis (CAD) systems can play an important role in lung cancer diagnosis as they can assist and facilitate the tedious, although relevant, work that have to be performed by the radiologists. The CAD systems is in general terms organized by 5 different progressive stages. In a first phase, a preprocessing stage can prepare the images for further analysis, by normalizing the scale or reduce the noise. A following stage can be an enhancement step to make more visible some structures, as lung nodules, to ease the detection phase. Nodule segmentation is the next step, to accurately define nodule boundaries.

Once the nodule is segmented, an adequate nodule characterization is crucial for analysis and cor-

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Table 1: Weights for the radiologists classification. 1^{st} row, the labels associated to each degree of malignancy. 2^{nd} row, p, the corresponding weight values.

Level of malignancy	1	2	3	4	5
Weight – p	0.15	0.15	0.20	0.25	0.25

responding malignancy differentiation. Measures of texture, gradient, shape or intensity information (Wu et al., 2013a; Akram et al., 2015; Liu et al., 2015) are usually applied in this context. Afterwards, feature selection can reduce the feature space, removing redundant and irrelevant features. This can be made by different strategies as, for example, the use of Fisher criterion and genetic algorithms for this purpose (Liu et al., 2015). Using this information, different classification strategies can be applied to distinguish the nodules regarding its malignancy. Different classifiers as Support Vector Machines (SVM) or Random Forest (RF), among others, were also used for this purpose (Kaya and Can, 2015). The best results in the stateof-the-art for malignancy nodule classification were presented by (Wu et al., 2013b) with a receiver operating characteristic (ROC) curve (AUC value) value of 91% by comparing the results with diagnosed nodules by either biopsy, follow-up or surgery.

The objective of this work was the development of a system that discriminate nodules by its malignancy using as reference annotated delineations of 4 radiologists.

2 MATERIALS

The dataset has images from the Lung Image Database Consortium and Image Database Resource Initiative (LIDC-IDRI) (Armato et al., 2011). The LIDC-IDRI is a public image dataset that includes diagnostic and lung cancer screening thoracic Computed Tomography scans with marked up, annotated lesions. These images contain a variable number of slices, where each slice has a resolution of 512×512 pixels.

Each one of the scans includes annotations provided by 4 different radiologists, who have assigned a degree of malignancy in a scale of 1 to 5 where 1 means "Highly Unlikely for Cancer" and 5 means "Highly Suspicious for Cancer". The opinions of the 4 radiologists diverge, and this happens quite often. For that reason, we selected nodules with a clear identification of the malignancy classification, leaving as indeterminate others with considerable divergence.

As each nodule has an assigned label from 4 radiologists, we combined the 4 labels by a weighted average of the individual labels. The estimated combined label of each sample, the degree of malignancy, M^i , of each nodule is defined by:

$$M = \sum_{k=1}^{4} \beta^k dm(k) \therefore \beta^k = p(k) \tag{1}$$

where p(k) is the weight value for each radiologist k and dm(k) is the assigned label m by the radiologist for the nodule.

Table 1 shows the weights that were used for p and each corresponding level of malignancy, m. In this case we employed higher values for higher degrees of malignancy, labels 4 and 5, as we assign higher relevance that a radiologists classify a nodule as highly suspicious of being malignant than lowers levels, that is, unlikely suspicious.

Therefore, a complete set of solid nodules that were annotated by 4 experienced radiologists were analyzed and used to construct the dataset. Hence, in the groundtruth we consider those nodules with a final score equal or higher to 4, as malignant45 (labels 4 and 5 correspond to significantly suspicious for cancer), or equal or lower than 2, as malignant12 (unlikely for cancer). The others are indeterminate.

Finally, the dataset resulted in a total of 177 malignant45 and 121 malignant12 nodules, in a total of 298 nodules.

3 METHODOLOGY

The process of diagnosis consists of the following main steps: feature measurement, feature selection, classification and validation. Once the pulmonary region of interest is delimited (Novo et al., 2014), the method takes, as input, the segmented nodules using an approach that was previously developed (Gonçalves et al., 2016). This approach uses the principle of central adaptive medialness previously proposed for lung nodule candidate detection task (Novo et al., 2015) that also demonstrates its robustness in nodule segmentation.

Regarding feature measurement, a set of 295 features was defined in order to include a large and diverse set of features that would be able to capture malignancy nodule properties. The feature set includes morphological (volume, compactness or sphericity, among others), intensity (different statistics) or texture features (Gray-Level CoOccurrence Matrix (GLCM), Gray-level intensity histogram (GLIH) or Gabor filters, among others.

Feature selection was the next step to identify the main useful characteristics for the classification avoiding, therefore, irrelevant and redundant features and facilitating the classification process. Feature selection was applied by 10-fold cross validation using 2 different algorithms: Correlation Feature Selection (CFS) that analyses the strength of a feature in predicting the class of the object; this approach tends to give little importance to the inter-correlation of the features; and Relief F algorithm, that samples instances randomly and checks the distance between them and the neighbours that have the same or different classes. A weight function uses the distances between the features to rank them (Hall, 1999).

Finally, different classifiers were evaluated using the selected features. In particular, three SVM classifiers were defined, using an exponential kernel as:

$$k(x,y) = exp\left(-\frac{\|x-y\|}{\theta}\right)$$
(2)

The SVMs used three values for θ , $\theta = [1, 2, 3]$, representing the degree of the exponential kernel. Three kNN classifiers with k = [13, 15, 17] were also included. The classification was performed by 10-fold cross-validation on the second set with 50 repetitions. The mean and standard deviation were calculated from the 50 values of AUC, using the selected subset of features.

4 RESULTS AND DISCUSSION

We trained and tested the method using the groundtruth dataset previously defined.

Regarding feature selection, by CFS algorithm, the features that appeared in more than 80% of the folds were selected and ranked according to the number of times they were selected. For the Relief F, the highest ranked features were chosen until the selected total was equal to the number of features selected by the CFS. The total number of features selected by both methods was 12. The majority of the features chosen by both methods were texture features, though CFS also selected two geometric features and Relief F three intensity features. The CFS selected a great number of GLCM and Laws features. CFS also included a volume and compactness characteristics, which is coherent as the radiologists tend to consider compact and round nodules as unlikely for cancer, or large and irregular nodules as suspicious for cancer. Relief F selected different features that pay attention to the center calcification of the nodules, property used for identifying nodule malignancy.

The main performance classification results are shown in Table 2 and Table 3. In general terms, the AUC values for all the classifiers and feature subsets are satisfactorily high, though there is no considerable difference between them. Even so, The SVM classifiers provide the best results outperforming all KNN classifiers, specially with the CFS subset. From all of them, the lowest value was obtained with the 13-KNN and CFS with an AUC of 93,2%. On the other hand, the SVMs results with CFS subset provided very similar results so it does not provide a clear conclusion on which classifier is the best. However, the third degree SVM is slightly better than the others, providing equivalent AUCs of 96,4% versus an 96,3% and 96,2% from the second and first degree classifiers, respectively.

The classification results can also be checked in the ROC curves of Figure 1 and Figure 2, where the previous evaluation comments remain. These ROC curves were constructed defining progressive thresholds in the *a priori* probabilities of the classifiers from 0 to 1, with a step of 0.01. Once again, the SVM classifiers are better than KNN classifiers and their performance is very similar. Although this is true, the subset from Relief F improves the results of the KNN and decreases the performance of the SVMs.

Different correct classification examples are shown in figure 3, with the corresponding degree of confidence. The degree of confidence is the posterior *probability* of a nodule belonging to a particular class (malignant12 or malignant45), that is, it identifies the degree of certainty that a classifier has on identifying a nodule as the corresponding malignant12 or malignant45 class. The left column represents malignant12 nodules and the right column represents the malignant45 ones. In each image the contour of the nodule is also presented giving a clear idea of their morphology, representing the color of the class label (green for malignant12 or red for malignant45). As observed in the statistical results, most of the nodules were satisfactorily classified. We also include examples of misclassifications in Figure 4. In the case of the first misclassification (case 72), the nodule presents a high degree of spiculation and large size, characteristics that mainly are observed in malignant45 nodules. In the case of the second misclassification (case 283) the small nodule has similar characteristics to malignant12 ones in terms of shape or size, but other relevant features are similar to malignant45 nodules which provokes the final malignant45 labeling.



Figure 1: ROC curves of the classification performances of the 6 classifiers and the 12 features selected by CFS algorithm.



Figure 2: ROC curves of the classification performances of the 6 classifiers and the 12 features selected by Relief-F algorithm.

True Label	Malignant12			Malignant45	
Case		Confidence (%)	Case		Confidence (%)
178		75,5	138		88,3
180		72,4	163		94,6
212		72,1	165		87,1
268		79,3	193		79,9
270		55,48	202		80,1 IONS
275		55,24	210		70,4
277		68,5	242		92,7

Figure 3: Examples of correct malignant12 (1^{st} column) and malignant45 (2^{nd} column) nodules class labels. Confidence is presented as the posterior probability of a nodule belonging to a particular class (malignant12 or malignant45).

5 CONCLUSIONS

This paper presents a system for the diagnosis of lung cancer by means of lung nodule malignancy classification in chest CT scans. The system has a set of 295 characteristics, being selected the most representative ones. Six KNN and SVM classifiers were evaluated. The best performance was achieved by a first order SVM with exponential kernel providing an AUC value of 96.2 \pm 0.5%, which are promising results.

In future work, new features can be included and wrapper based feature selection methods should be tested, as better results can be achieved by embedding the classifiers in the selection process the classifiers. Table 2: Classification results presented as the mean and standard deviation of 50 AUC % values, for 12 features selected by 2 model searches and 3 KNNs.

Area under curve, AUC (%)	13-KNN	15-KNN	17-KNN
Correlation Feature Selection, CFS	93.2 ± 0.8	93.5 ± 0.9	94.1 ± 0.7
Relief F	94.7 ± 0.7	94.4 ± 0.8	94.4 ± 0.7

Table 3: Classification results presented as the mean and standard deviation of 50 AUC % values, for 12 features selected by 2 model searches and 3 SVMs.

Area under curve, AUC (%)	1-SVM	2-SVM	3-SVM
Correlation Feature Selection, CFS	96.2 ± 0.5	96.3 ± 0.6	96.4 ± 0.5
Relief F	96.0 ± 0.6	96.3 ± 0.6	96.2 ± 0.6



Figure 4: Examples of incorrect malignant12 (1^{st} column) and malignant45 (2^{nd} column) nodules class labels. Confidence is presented as the posterior probability of a nodule belonging to a particular class (malignant12 or malignant45).

Also, other classifiers like neural networks should be implemented for classification comparison.

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REFERENCES

- Akram, S., Javed, M., Hussain, A., Riaz, F., and Akram, M. (2015). Intensity-based statistical features for classification of lungs ct scan nodules using artificial intelligence techniques. *Journal of Experimental and Theoretical Artificial Intelligence*, 27:737–751.
- Armato, S., McLennan, G., Bidaut, L., McNitt-Gray, M., Meyer, C., Reeves, A., Zhao, B., Aberle, D., Henschke, C., Hoffman, E., Kazerooni, E., MacMahon, H., Beeke, E. V., Yankelevitz, D., Biancardi, A., Bland, P., Brown, M., Engelmann, R., Laderach, G., Max, D., Pais, R., Qing, D., Roberts, R., Smith, A.,

Starkey, A., Batrah, P., Caligiuri, P., Farooqi, A., Gladish, G., Jude, C., Munden, R., Petkovska, I., Quint, L., Schwartz, L., Sundaram, B., Dodd, L., Fenimore, C., Gur, D., Petrick, N., Freymann, J., Kirby, J., Hughes, B., Casteele, A., Gupte, S., Sallamm, M., Heath, M., Kuhn, M., Dharaiya, E., Burns, R., Fryd, D., Salganicoff, M., Anand, V., Shreter, U., Vastagh, S., and Croft, B. (2011). The lung image database consortium (LIDC) and image database resource initiative (IDRI): a completed reference database of lung nodules on CT scans. *Medical Physics*, 38:915–931.

- Breadsmoore, C. J. and Screaton, N. J. (2003). Classification, staging and prognosis of lung cancer. *European Journal of Radiology*, 45:8–17.
- Gonçalves, L., Novo, J., and Campilho, A. (2016). Hessian based approaches for 3D lung nodule segmentation. *Expert Systems with Applications*, 61:1–15.
- Hall, M. A. (1999). *Correlation-based feature selection for machine learning*. PhD thesis, The University of Waikato.
- Kaya, A. and Can, A. (2015). A weighted rule based method for predicting malignancy of pulmonary nodules by nodule characteristics. *Journal of Biomedical Informatics*, 56:69–79.
- Liu, X., Ma, L., Song, L., Zhao, Y., Zhao, X., and Zhou, C. (2015). Recognizing common ct imaging signs of lung diseases through a new feature selection method based on fisher criterion and genetic optimization. *IEEE Journal of Biomedical and Health Informatics*, 19:635–647.
- Novo, J., Gonçalves, L., Mendonça, A., and Campilho, A. (2015). 3D lung nodule candidates detection in mul-

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tiple scales. IAPR International Conference on Machine Vision Applications, MVA 2015, pages 5–8.

- Novo, J., Rouco, J., Mendonça, A., and Campilho, A. (2014). Reliable lung segmentation methodology by including juxtapleural nodules. *International Conference on Image Analysis and Recognition, ICIAR 2014. Lecture Notes in Computer Science: Image Analysis and Recognition,* 8815:227–235.
- Siegel, R. L., Miller, K. D., and Jemal, A. (2016). Cancer statistics, 2016. CA: A Cancer Journal for Clinicians, 66:7–30.
- van Ginneken, B. (2008). Computer-aided diagnosis in thoracic computed tomography. *Imaging Decisions MRI*, 12:11–22.
- Wu, H., Sun, T., Wang, J., Li, X., Wang, W., Huo, D., Lv, P., He, W., Wang, K., and Guo, X. (2013a). Combination of radiological and gray level co-occurrence matrix textural features used to distinguish solitary pulmonary nodules by computed tomography. *Society for Imaging Informatics in Medicine*, 26:797–802.
- Wu, H., Sun, T., Wang, J., Li, X., Wang, W., Huo, D., Lv, P., He, W., Wang, K., and Guo, X. (2013b). Combination of radiological and gray level co-occurrence matrix textural features used to distinguish solitary pulmonary nodules by computed tomography. *Society for Imaging Informatics in Medicine*, 26:797–802.